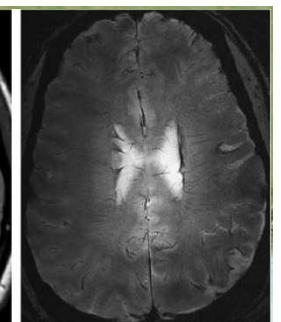
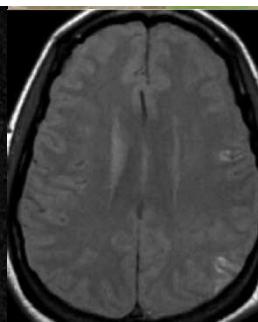
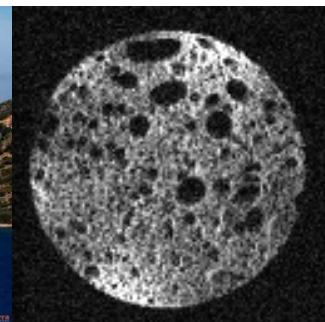
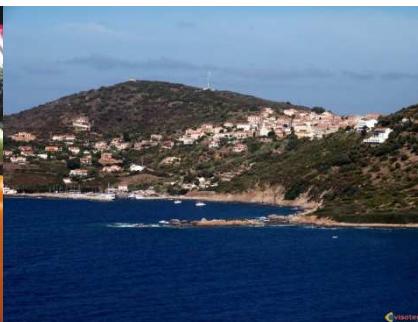




# Imagerie RMN

## Les bases du codage spatial

J.M. BONNY



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# Introduction

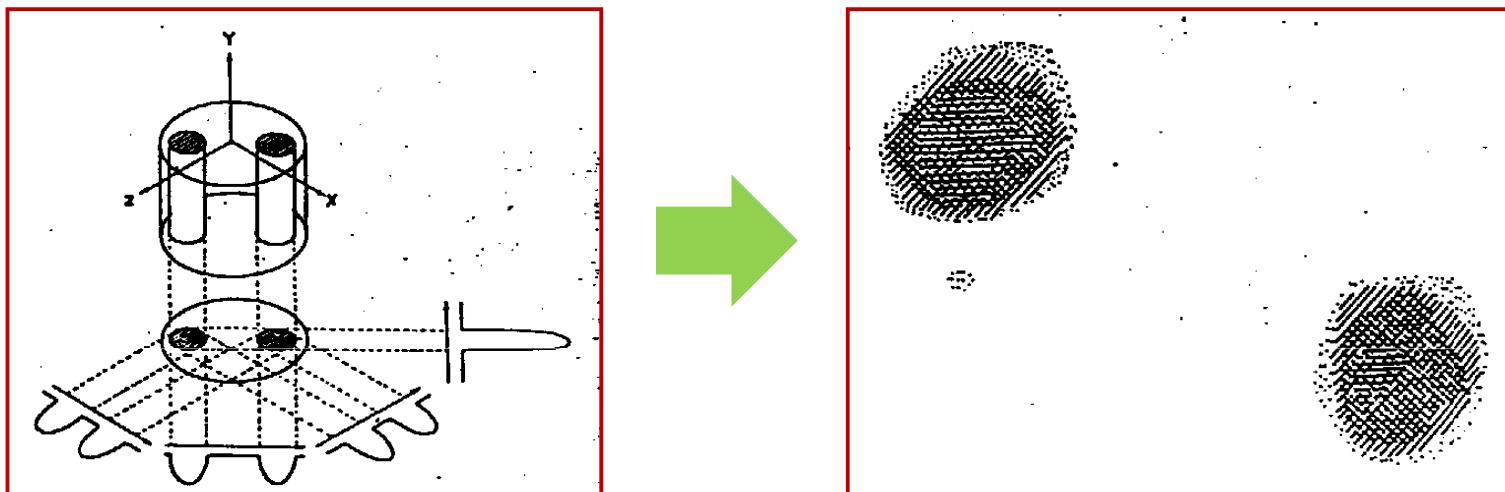


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# Rappels historiques

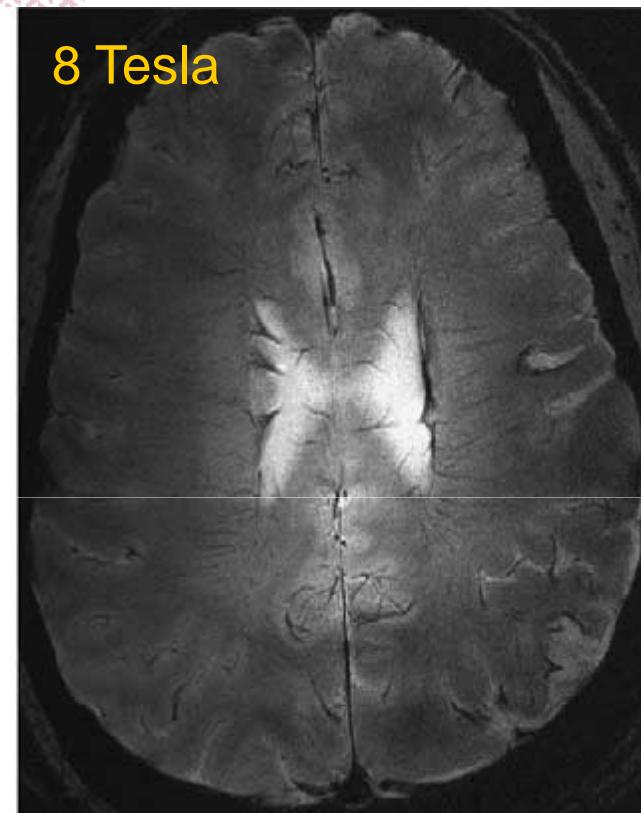
Première image de Lauterbur en 1973



Prix Nobel de Physiologie ou Médecine en 2003

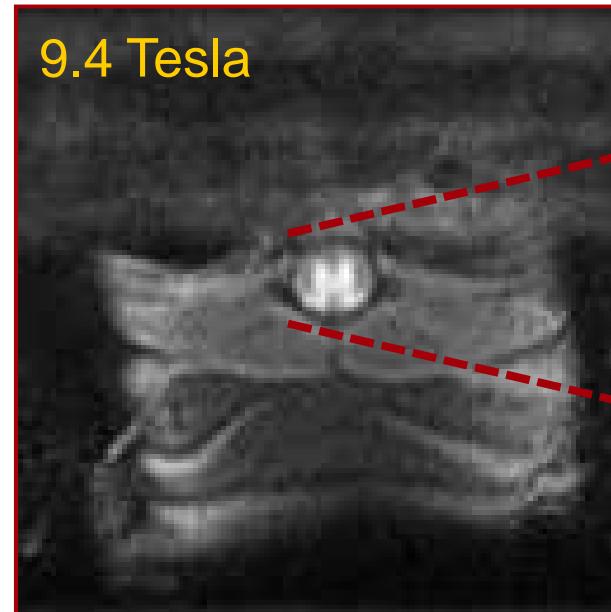
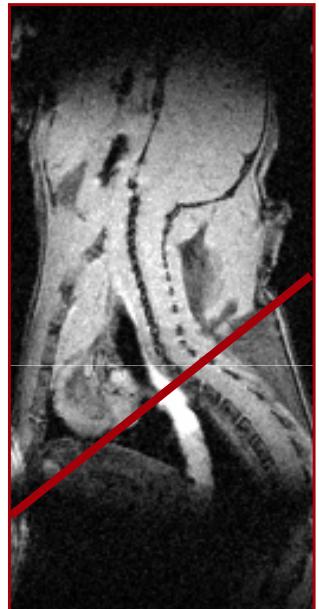
Lauterbur et Mansfield "for their discoveries concerning magnetic resonance imaging"

# Quelques exemples ...



Novak *et al.*, *Magn. Reson. Imaging* (2005)

# Quelques exemples ...



Bonny *et al.*, *Neurobiol. Dis.* (2004)

# Objectifs

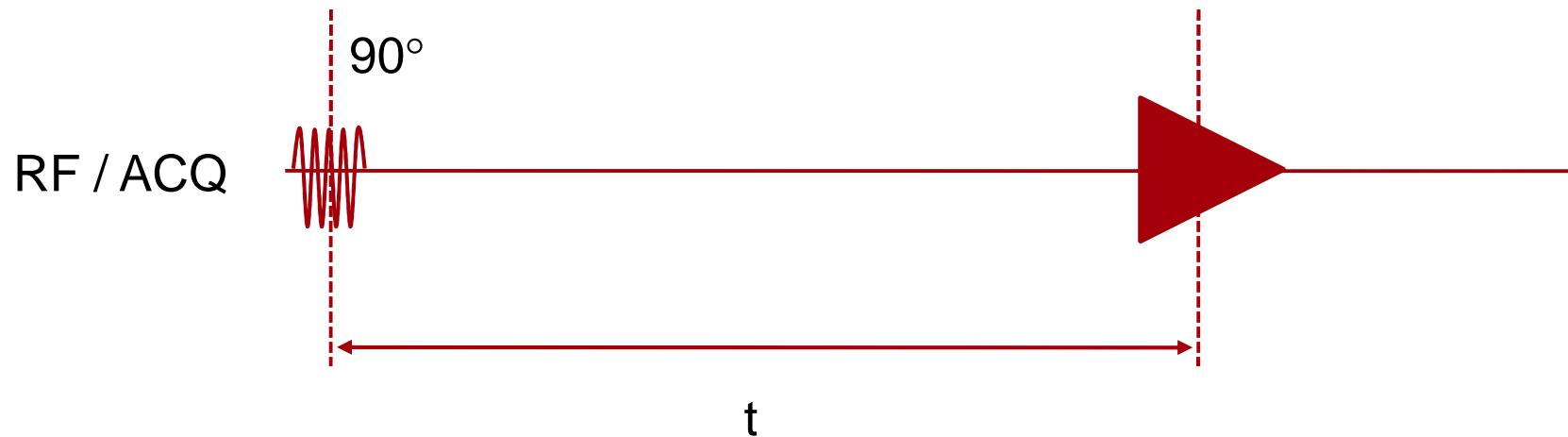
Comment obtenir (rapidement) plusieurs signaux RMN localisés ?

Outils permettant de décrypter la plupart des méthodes de codage spatial

- Balayage de l'espace k
- Sélection de tranche

Manipulation des contrastes pas abordée

# Séquence de base



Signal d'induction libre (SIL ou *FID*)

## Signal obtenu

Signal RMN au point  $\mathbf{r}$  après détection en quadrature

$$S(\mathbf{r}, t) = \rho(\mathbf{r}) \exp[i\phi(\mathbf{r}, t)]$$

Démodulation par rapport à  $\omega_0$

$$\phi(\mathbf{r}, t) = \int_0^t [\omega(\mathbf{r}, t') - \omega_0] dt'$$

Signal provenant de l'échantillon sans codage spatial

$$S(t) = \int \rho(\mathbf{r}) \exp[i\phi(\mathbf{r}, t)] d\mathbf{r}$$

$$S(t) = \int \rho(\mathbf{r}) d\mathbf{r} \quad \text{Si } \omega(\mathbf{r}) = \omega_0$$



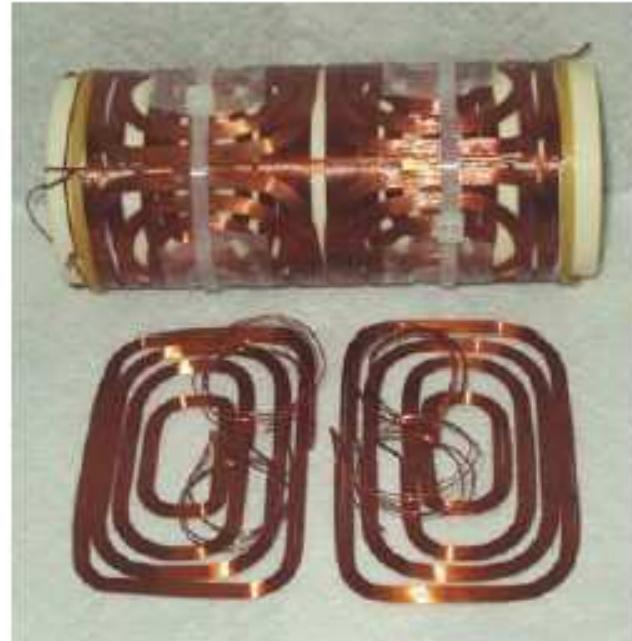
# Signal RMN en présence de gradient de champ magnétique



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# Les bobines de gradient



[http://www.dotynmr.com/mri/mri\\_fcgcpg.htm](http://www.dotynmr.com/mri/mri_fcgcpg.htm)

GERM Cargèse 2008

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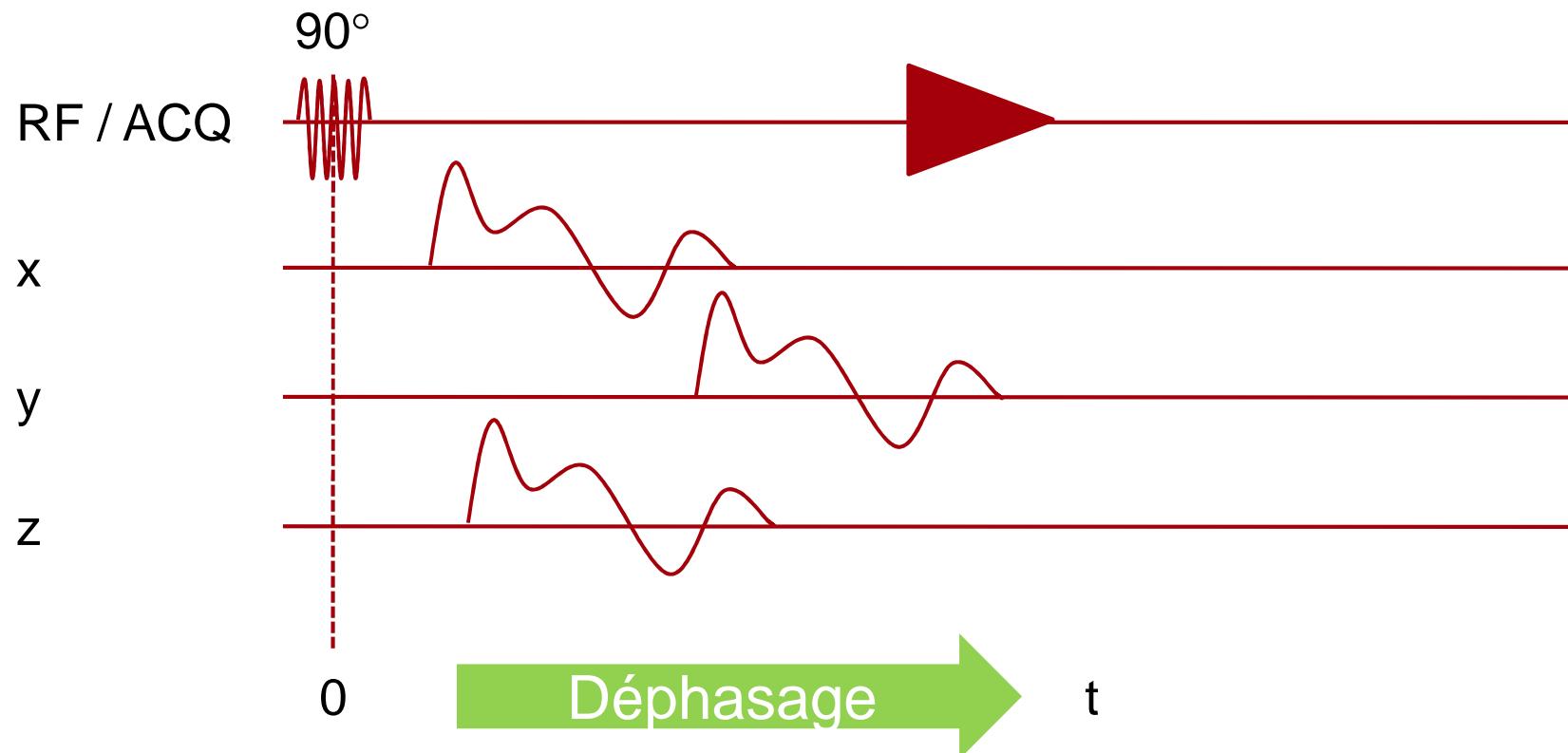
# Effet des bobines de gradient

$$\mathbf{G}(t) = \begin{bmatrix} G_x(t) \\ G_y(t) \\ G_z(t) \end{bmatrix} = \begin{bmatrix} \frac{\partial B}{\partial x}(\mathbf{r}, t) \\ \frac{\partial B}{\partial y}(\mathbf{r}, t) \\ \frac{\partial B}{\partial z}(\mathbf{r}, t) \end{bmatrix}$$

$$\omega(\mathbf{r}, t) = \mathbf{G} \cdot \mathbf{r} + \omega_0 = \gamma [G_x(t)x + G_y(t)y + G_z(t)z] + \omega_0$$

A l'origine du repère "image"    $\omega(0, t) = \omega_0$

# Séquence en présence de gradients



# Signal obtenu

Phase en  $\mathbf{r}$  à  $t$

$$\phi(\mathbf{r}, t) = \int_0^t [\omega(\mathbf{r}, t') - \omega_0] dt' = \gamma \int_0^t \mathbf{G}(t') \cdot \mathbf{r} dt' = 2\pi \mathbf{r} \cdot \mathbf{k}(t)$$

avec

$$\mathbf{k}(t) = \frac{\gamma}{2\pi} \int_0^t \mathbf{G}(t') dt'$$

Signal provenant de l'échantillon

$$S(t) = \int \rho(\mathbf{r}) \exp[2\pi i \mathbf{r} \cdot \mathbf{k}(t)] d\mathbf{r}$$



# Trajectoires dans l'espace réciproque (ou espace k)



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# L'espace k

$$S(t) = \int \rho(\mathbf{r}) \exp[2\pi i \mathbf{r} \cdot \mathbf{k}(t)] d\mathbf{r}$$

Représentation du signal dans l'espace k

- Espace Cartésien
- Coordonnées ( $k_x, k_y, k_z$ )
- Signal en t représenté par le point de coordonnées ( $\mathbf{k}(t), S(t)$ )

$G(t)$    $\mathbf{k}(t)$  Trajectoire dans l'espace k

$S(t)$  Valeur du point de coordonnées  $\mathbf{k}(t)$

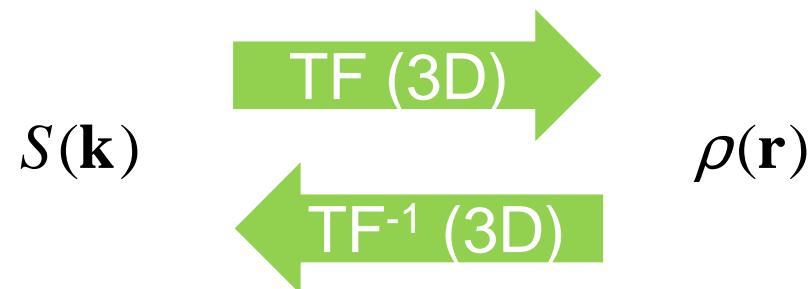
# Intérêt de l'espace k

Par définition

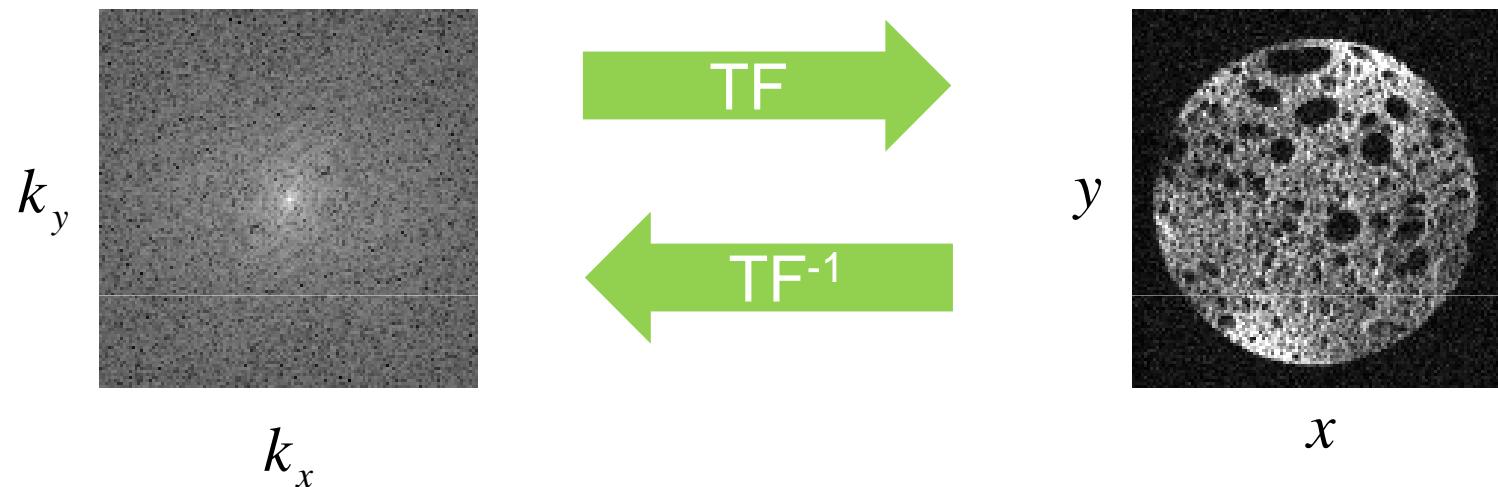
$$S(\mathbf{k}) = \int \rho(\mathbf{r}) \exp(2\pi i \mathbf{r} \cdot \mathbf{k}) d\mathbf{r} = \mathbf{F}^{-1}(\rho(\mathbf{r}))$$

$$\mathbf{F}(S(\mathbf{k})) = \mathbf{F} \circ \mathbf{F}^{-1}(\rho(\mathbf{r})) = \rho(\mathbf{r})$$

Espace k réciproque de l'espace image



# Espace k / Espace image



# Principe général



Evolution temporelle du gradient  $\mathbf{G}_i(t)$



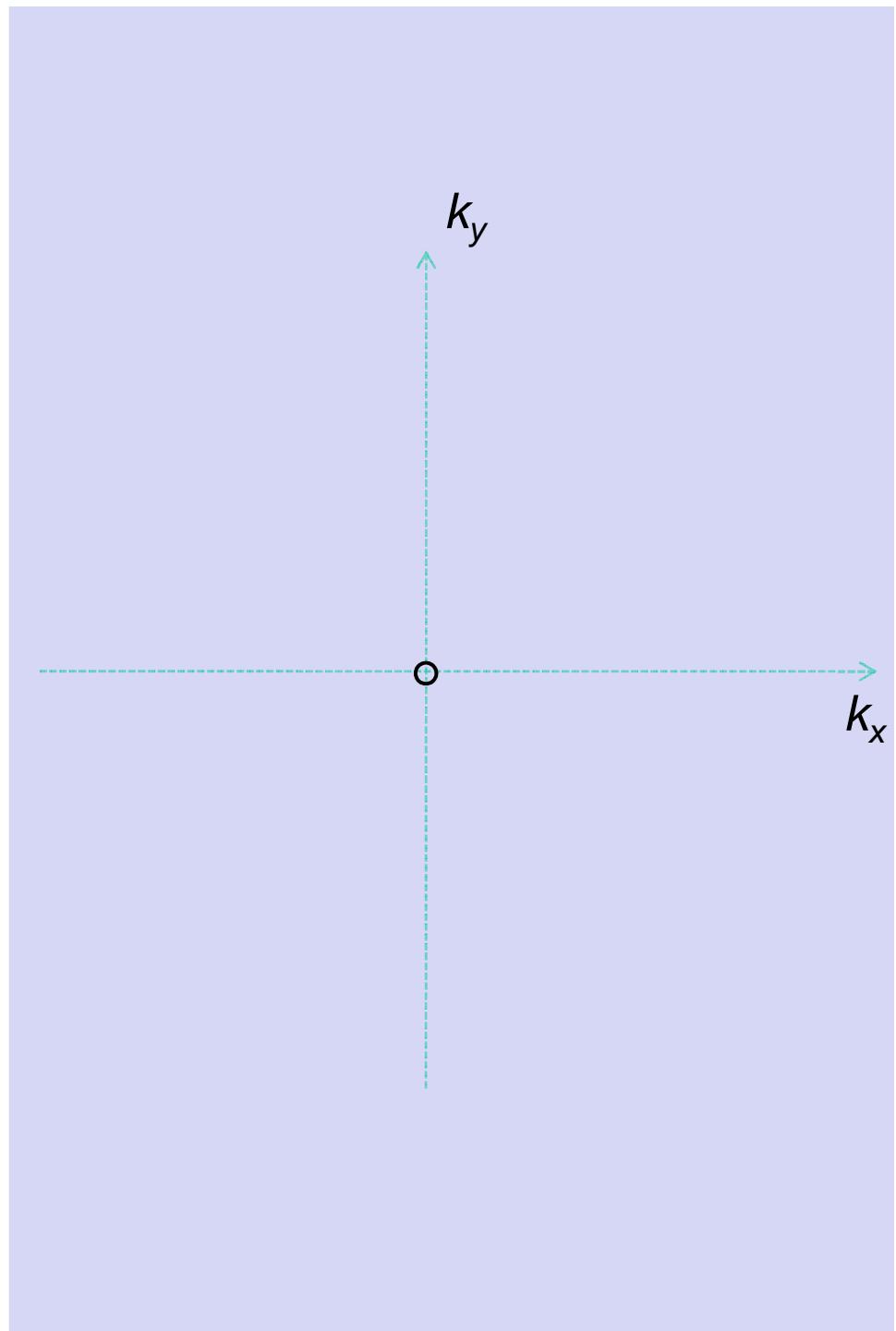
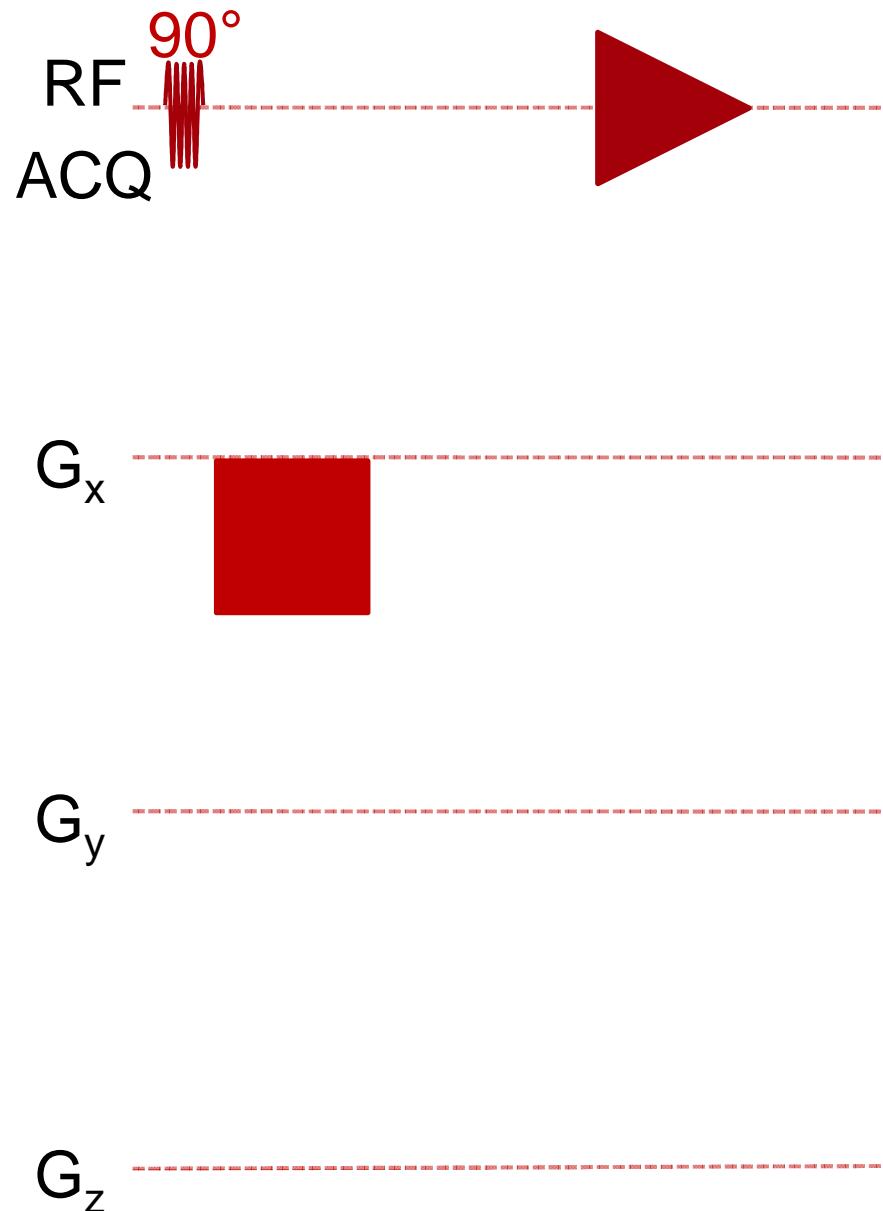
$$\text{Trajectoire } \mathbf{k}_i(t) = \frac{\gamma}{2\pi} \int_0^t \mathbf{G}_i(t') dt'$$

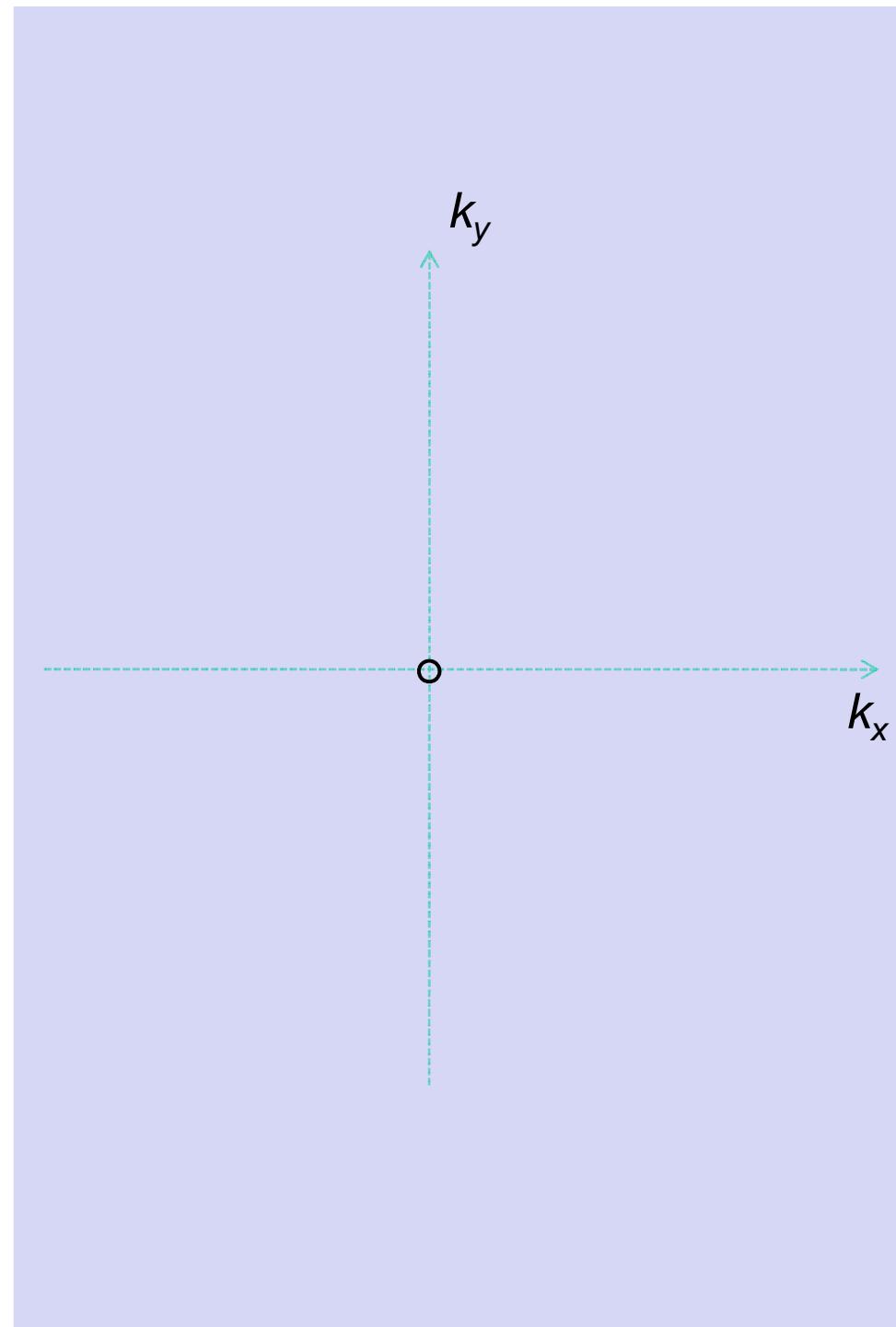
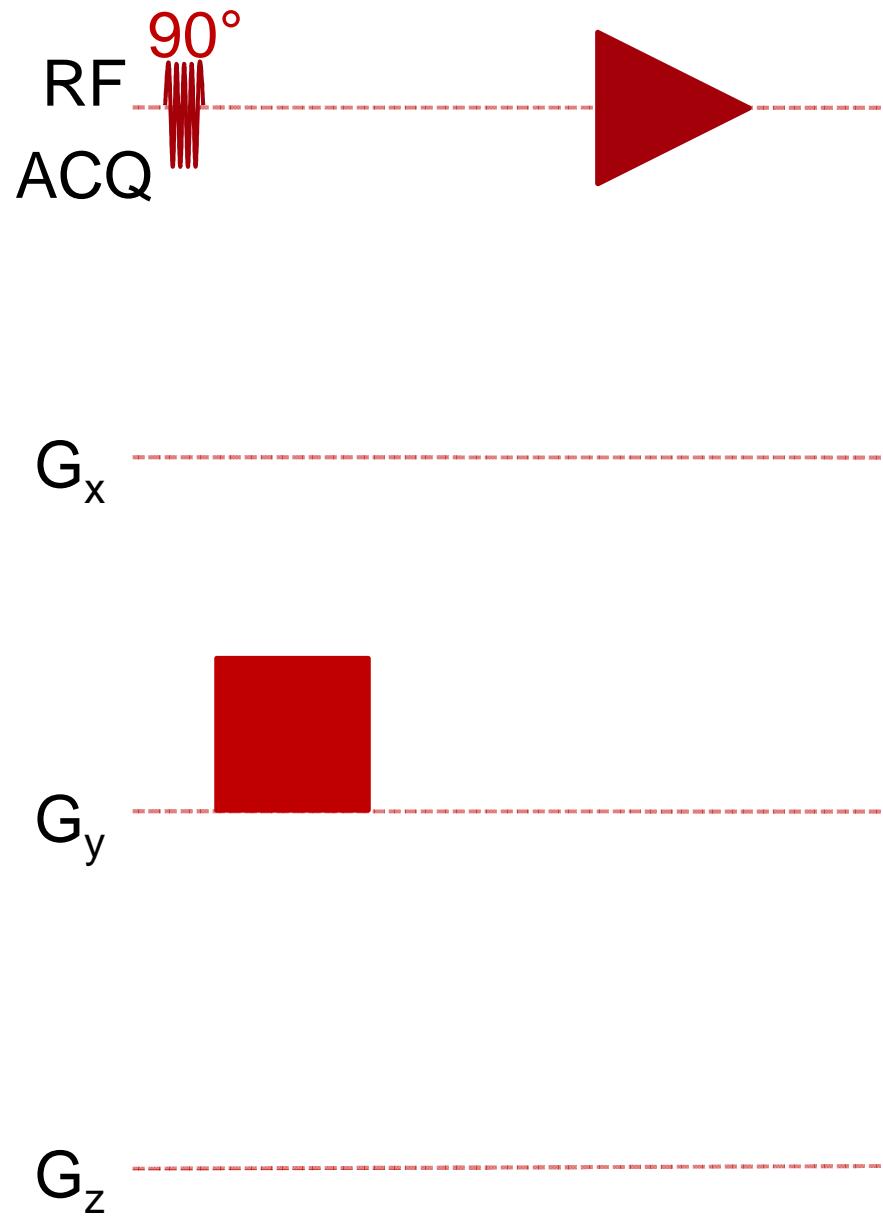


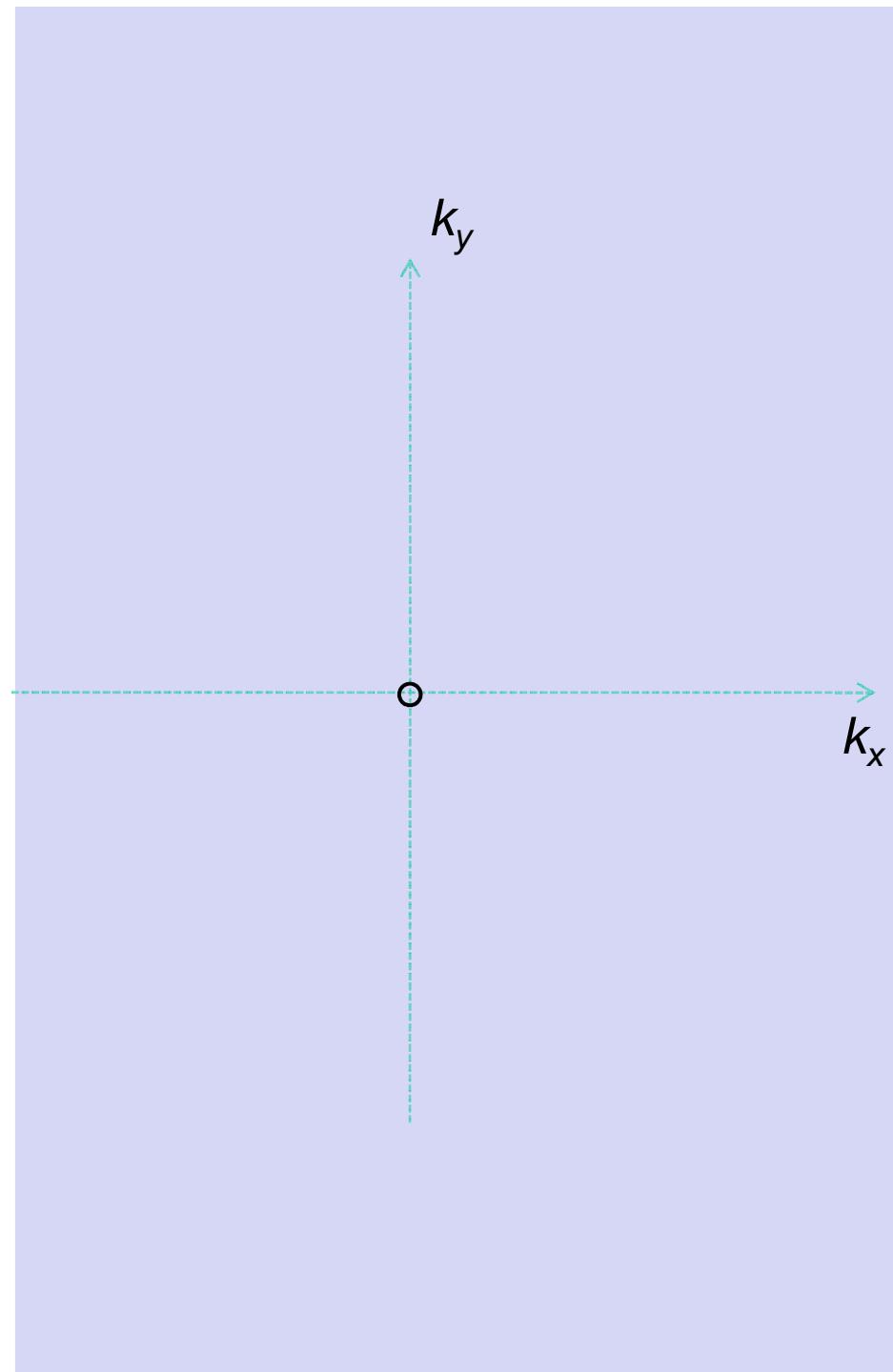
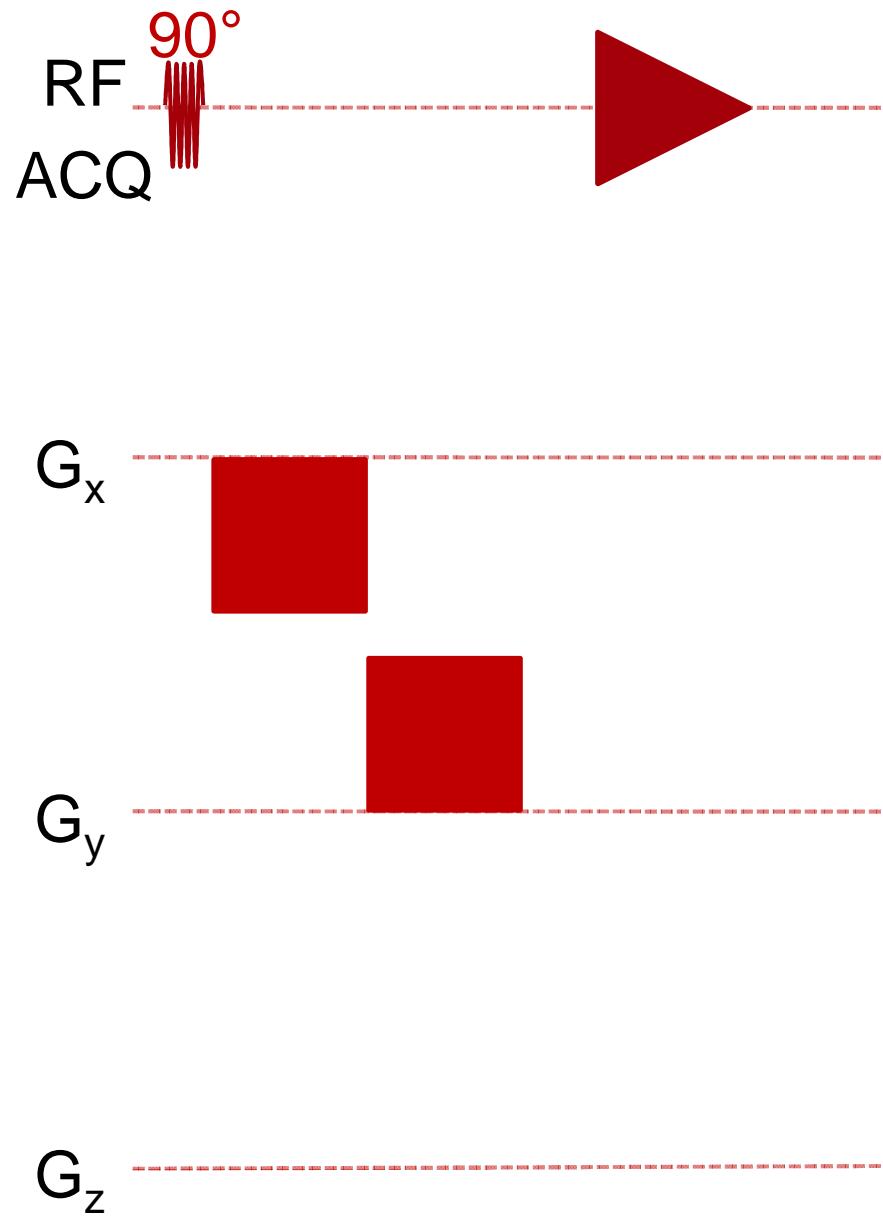
Remplissage de l'espace k

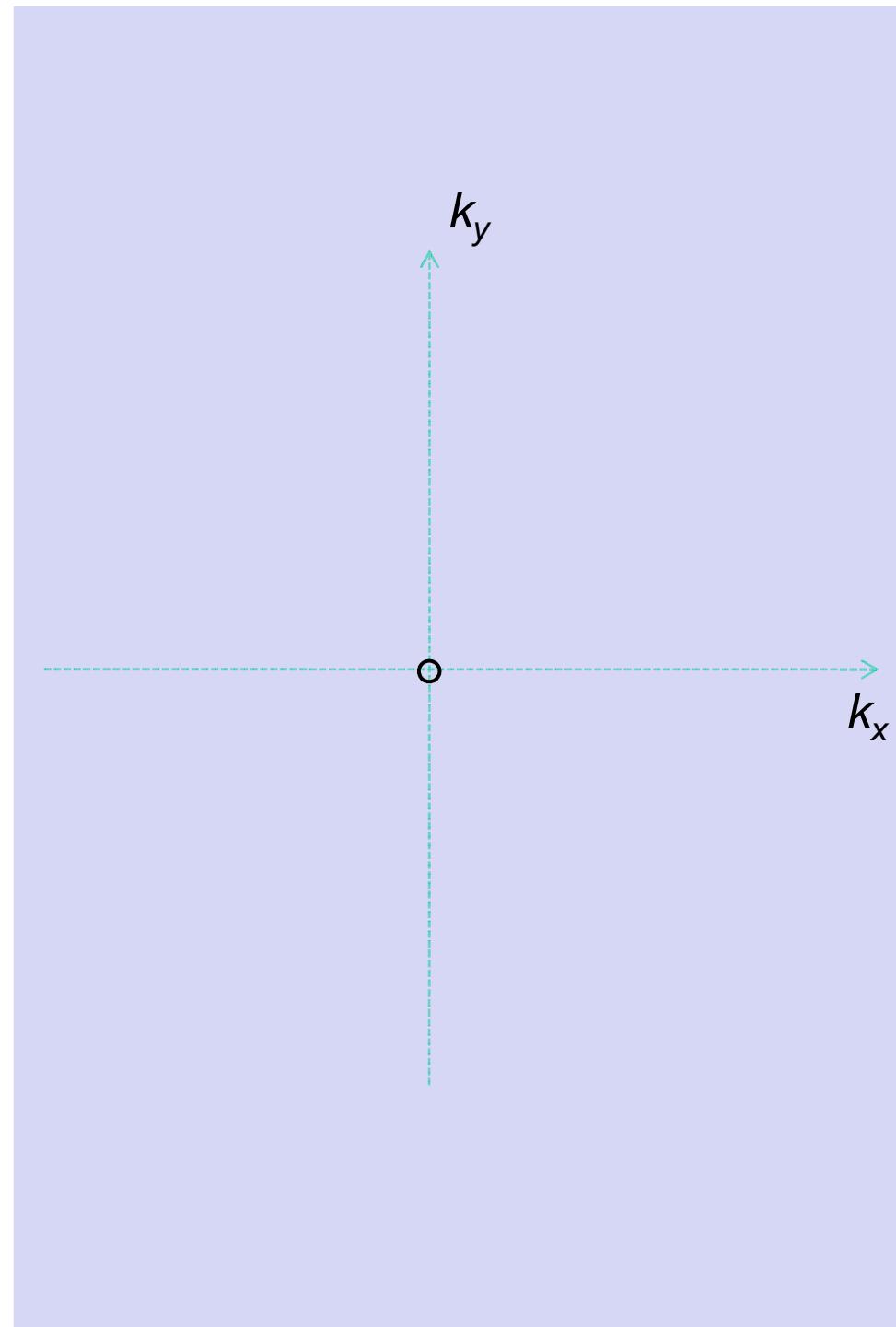
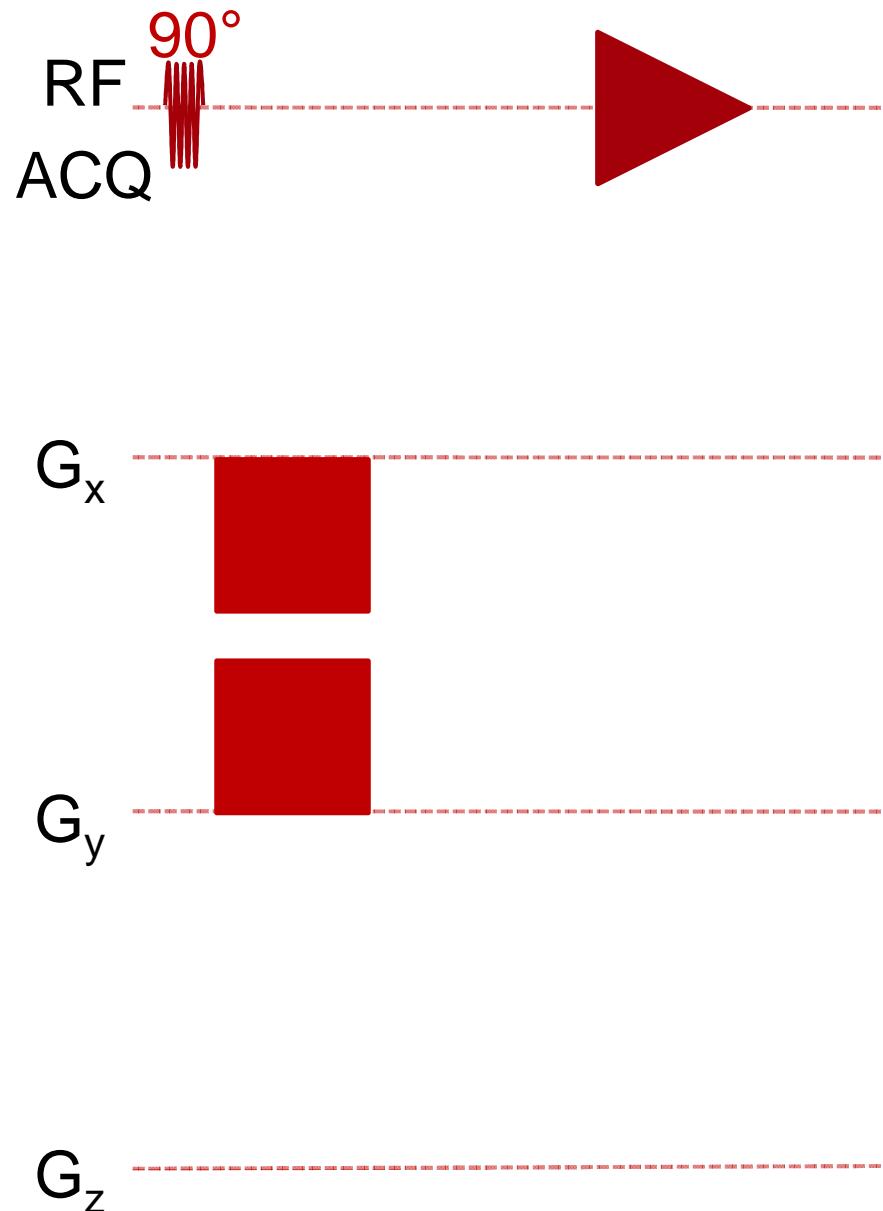


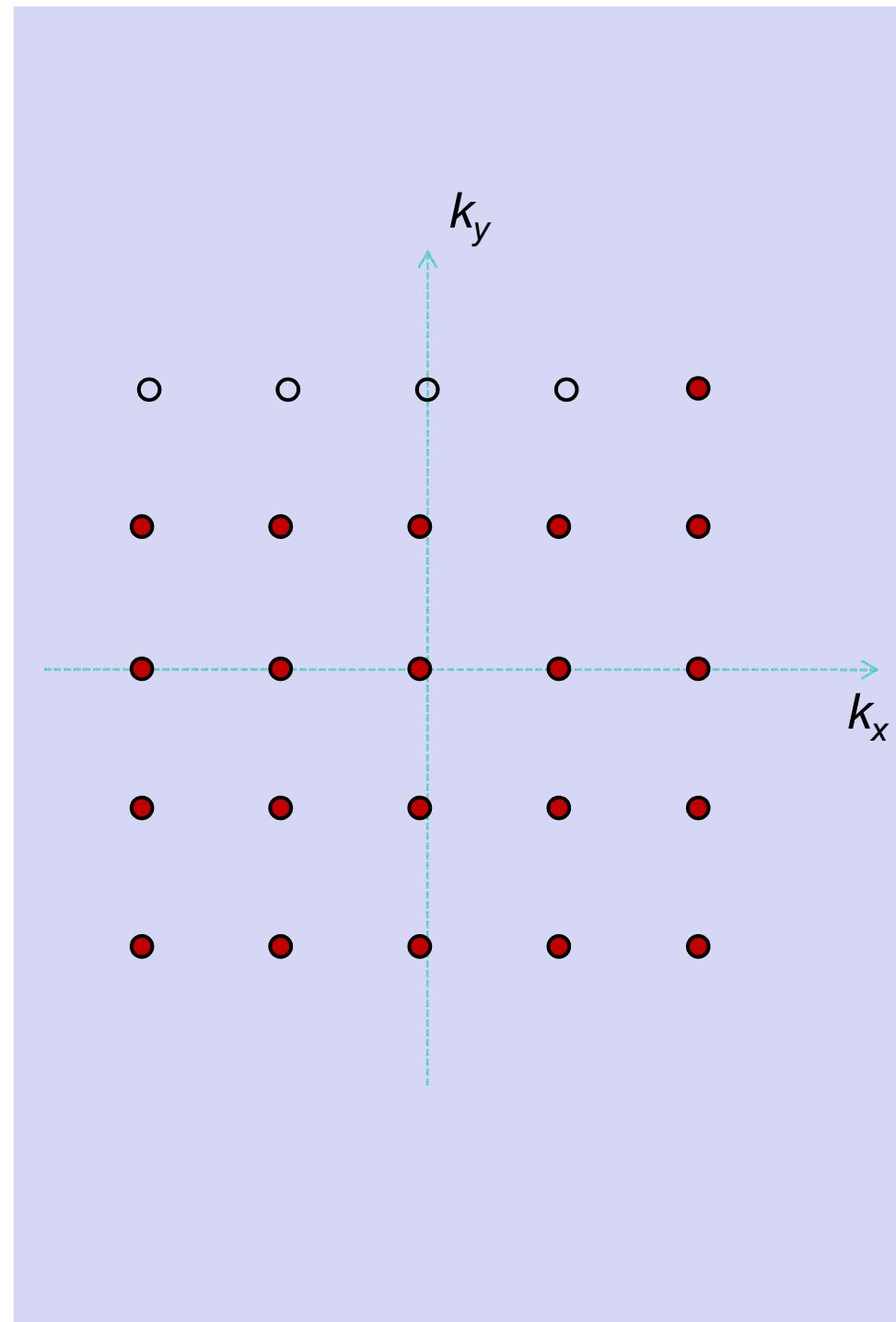
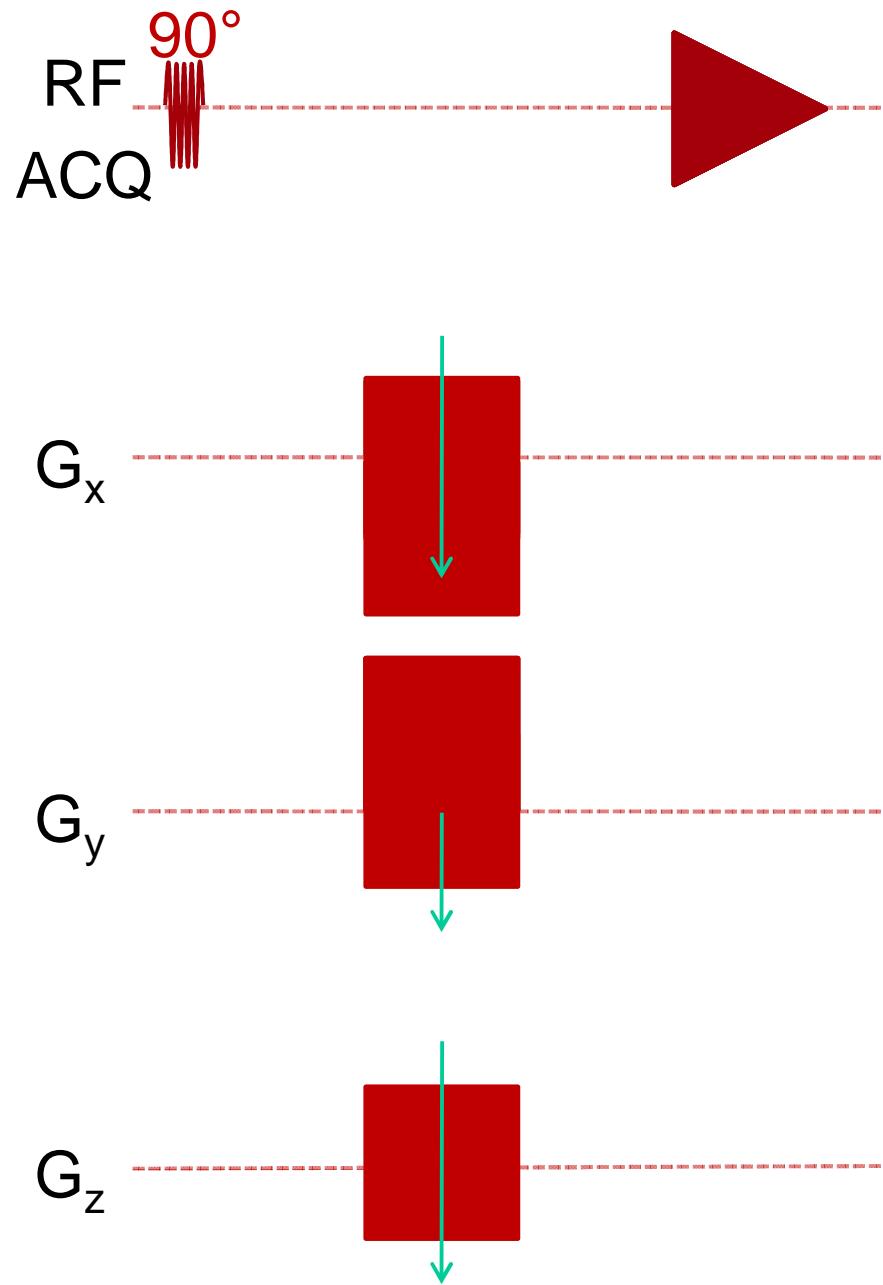
Image











# *Pure phase encoded imaging*

Balayage Cartésien de l'espace k

Gradients précédant l'acquisition

- Gradient de codage de phase
- Codage des 3 directions

Différents modes d'acquisition

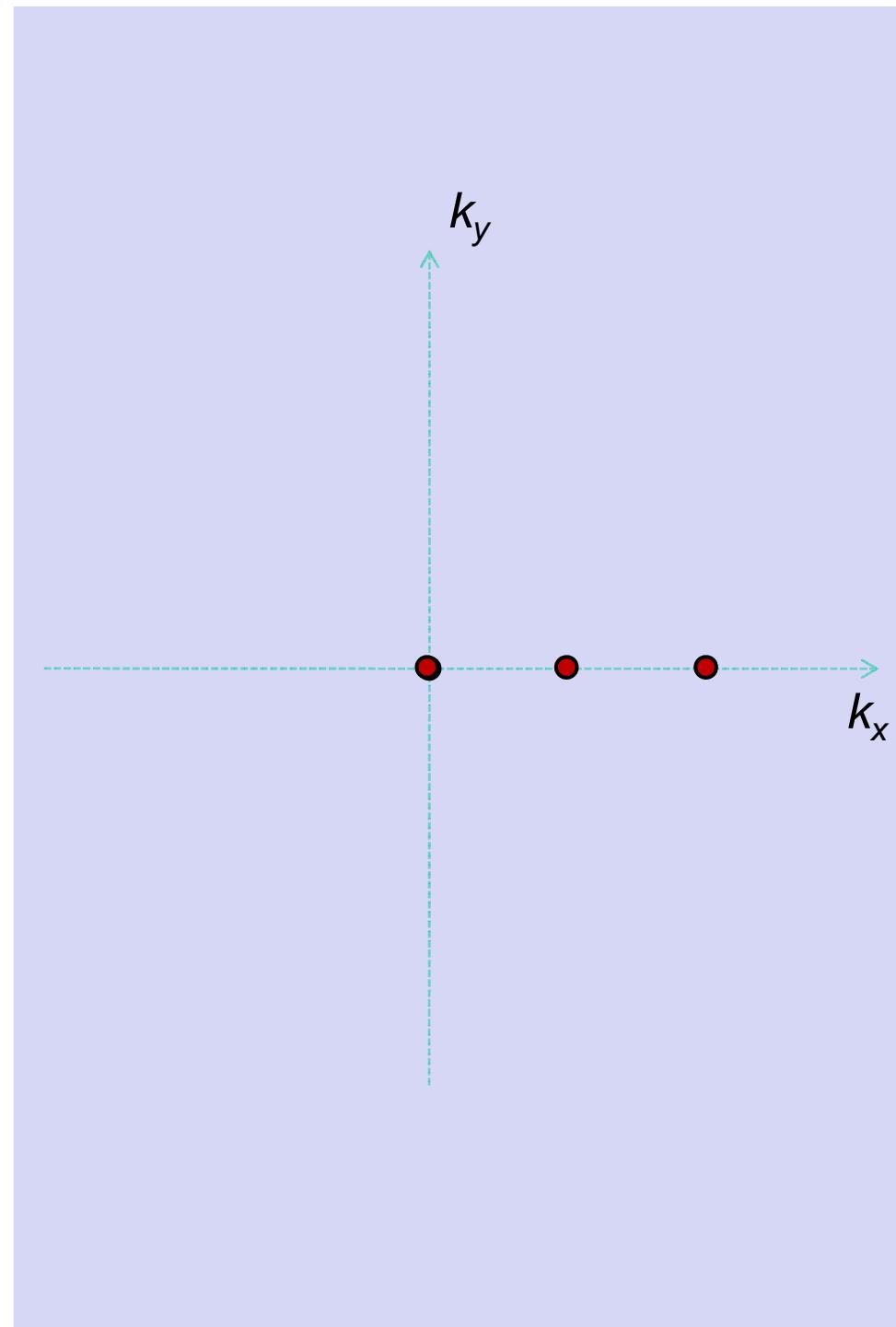
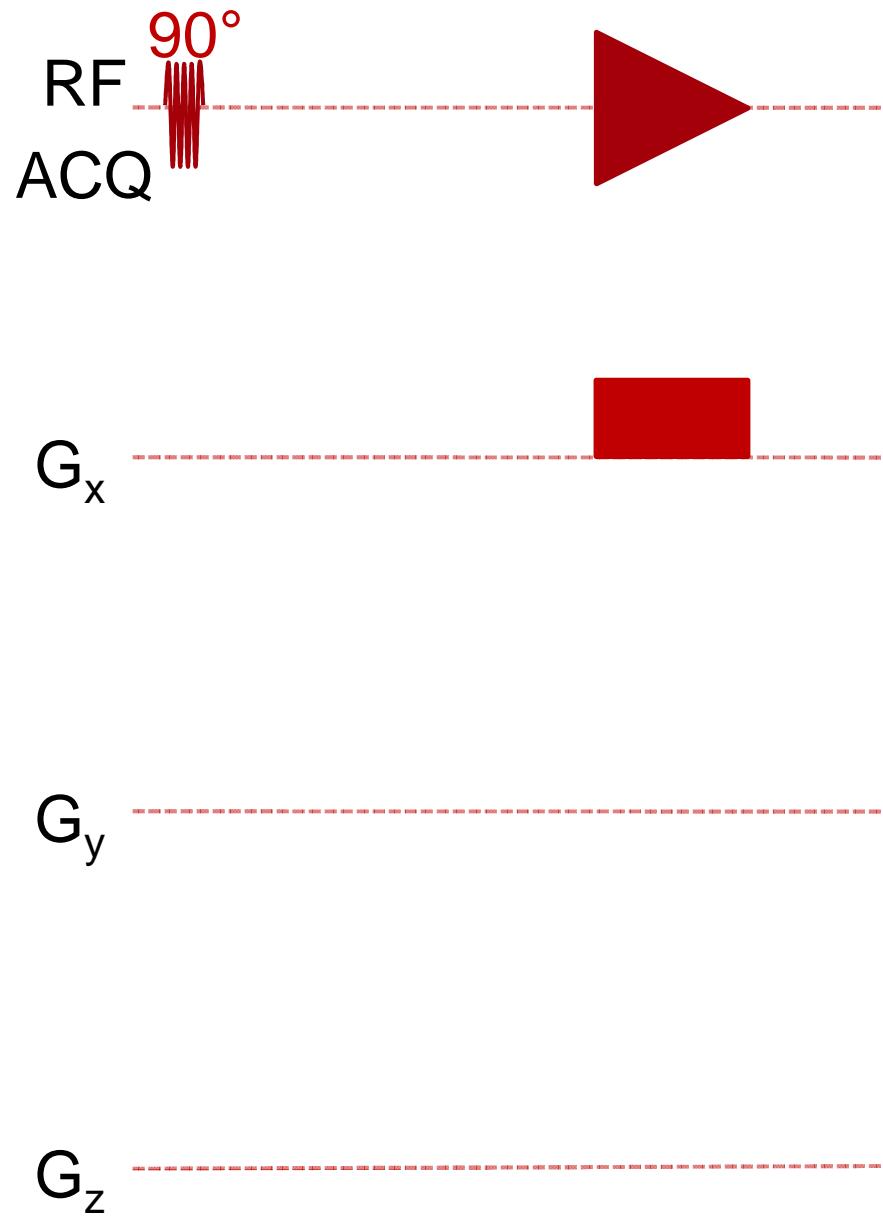
- Un point du SIL
- FID complet

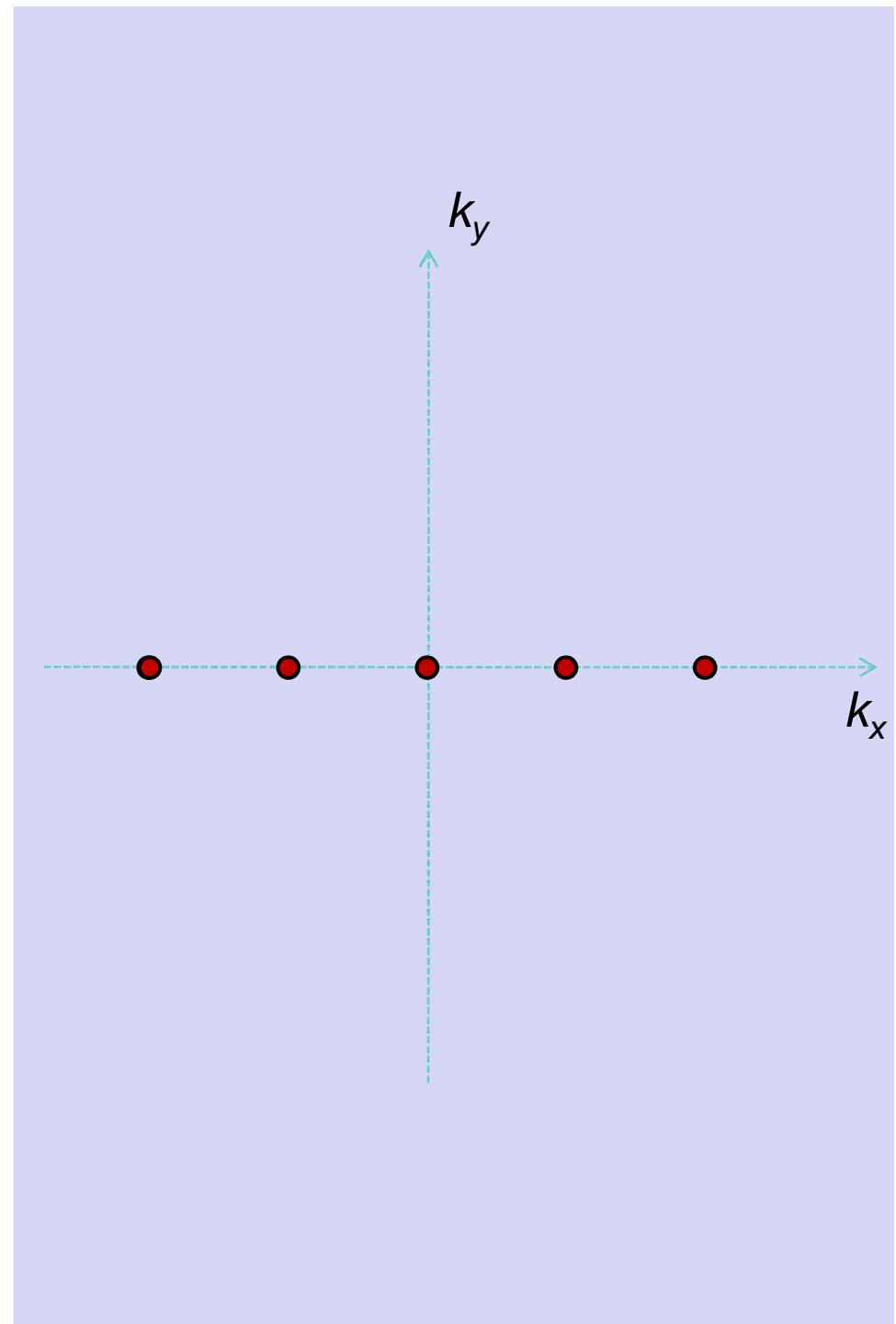
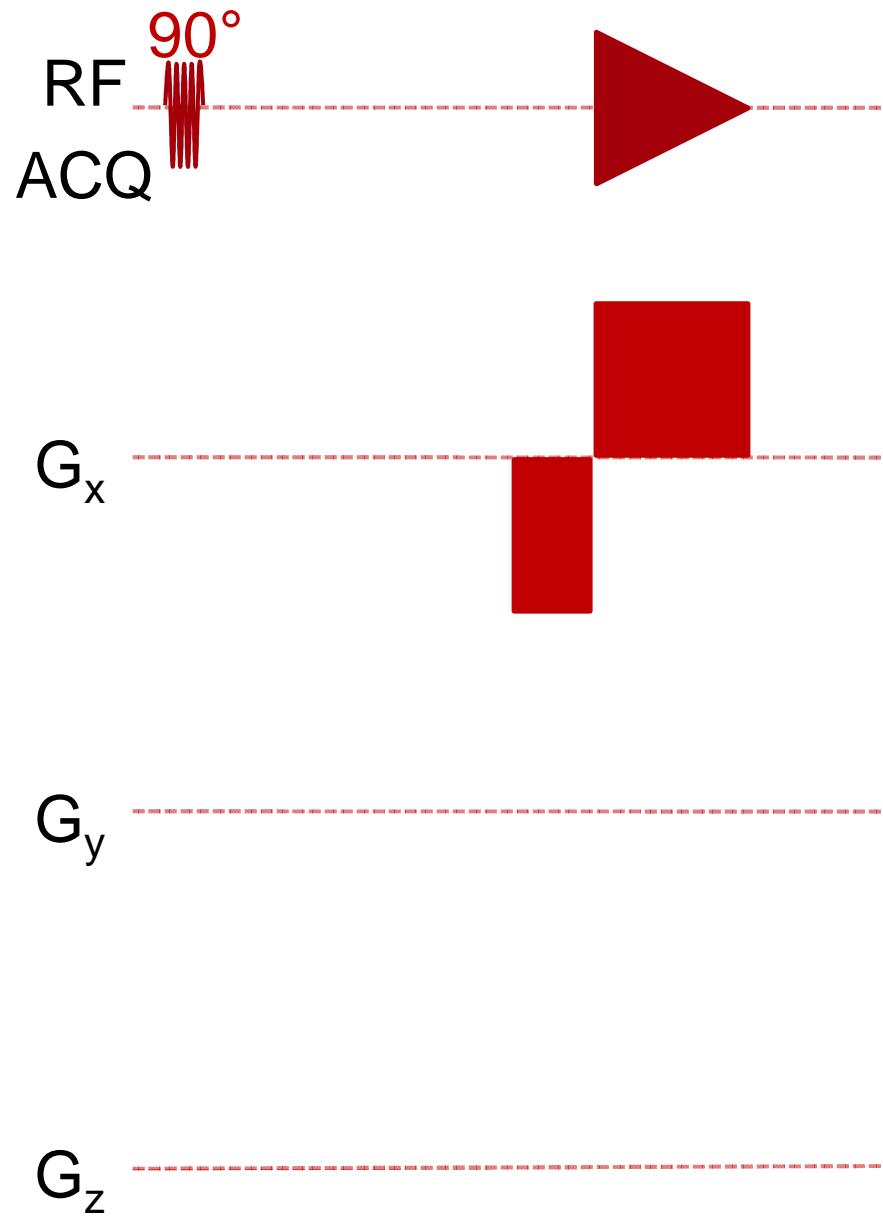
*Single Point Imaging*  
*Chemical Shift Imaging*

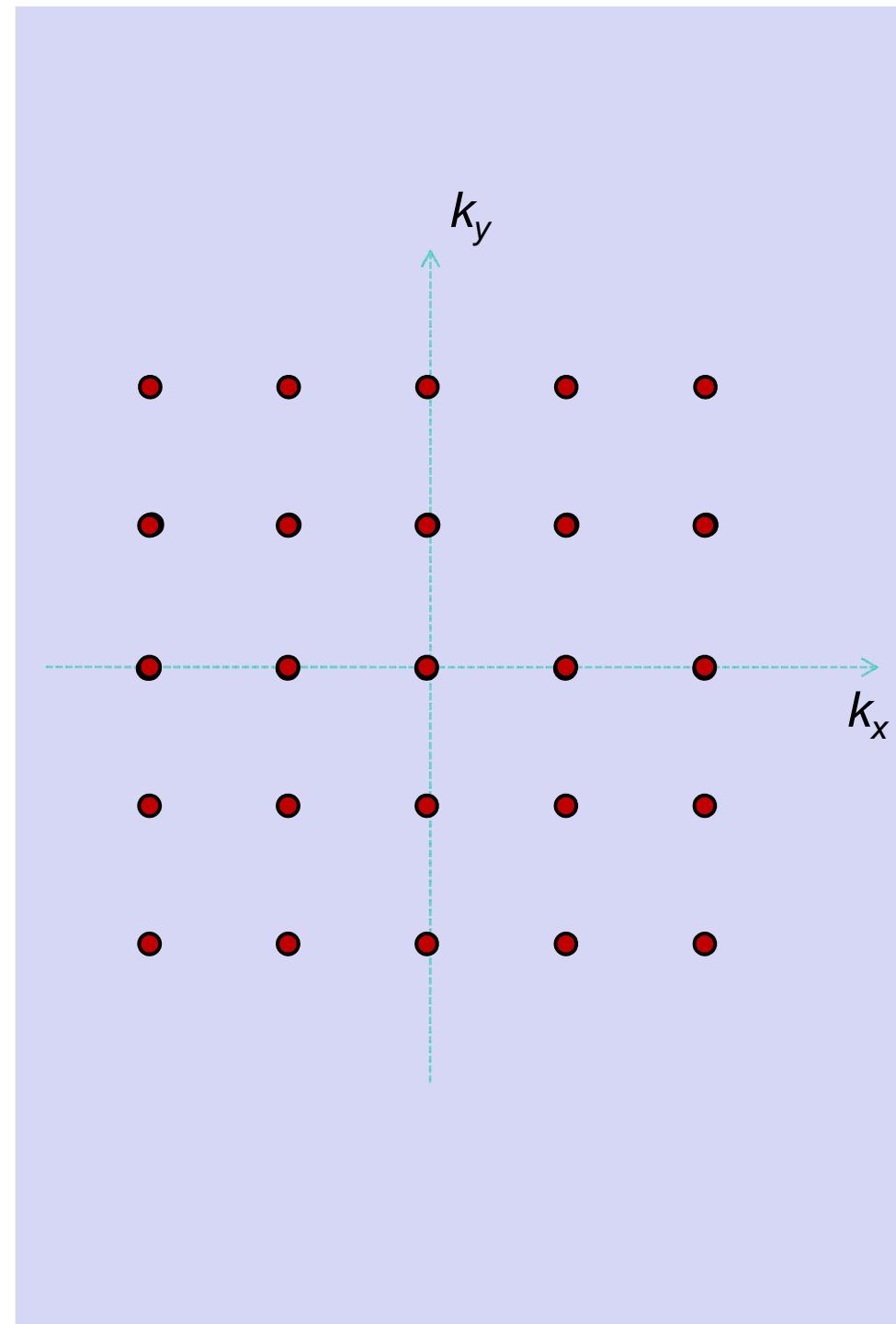
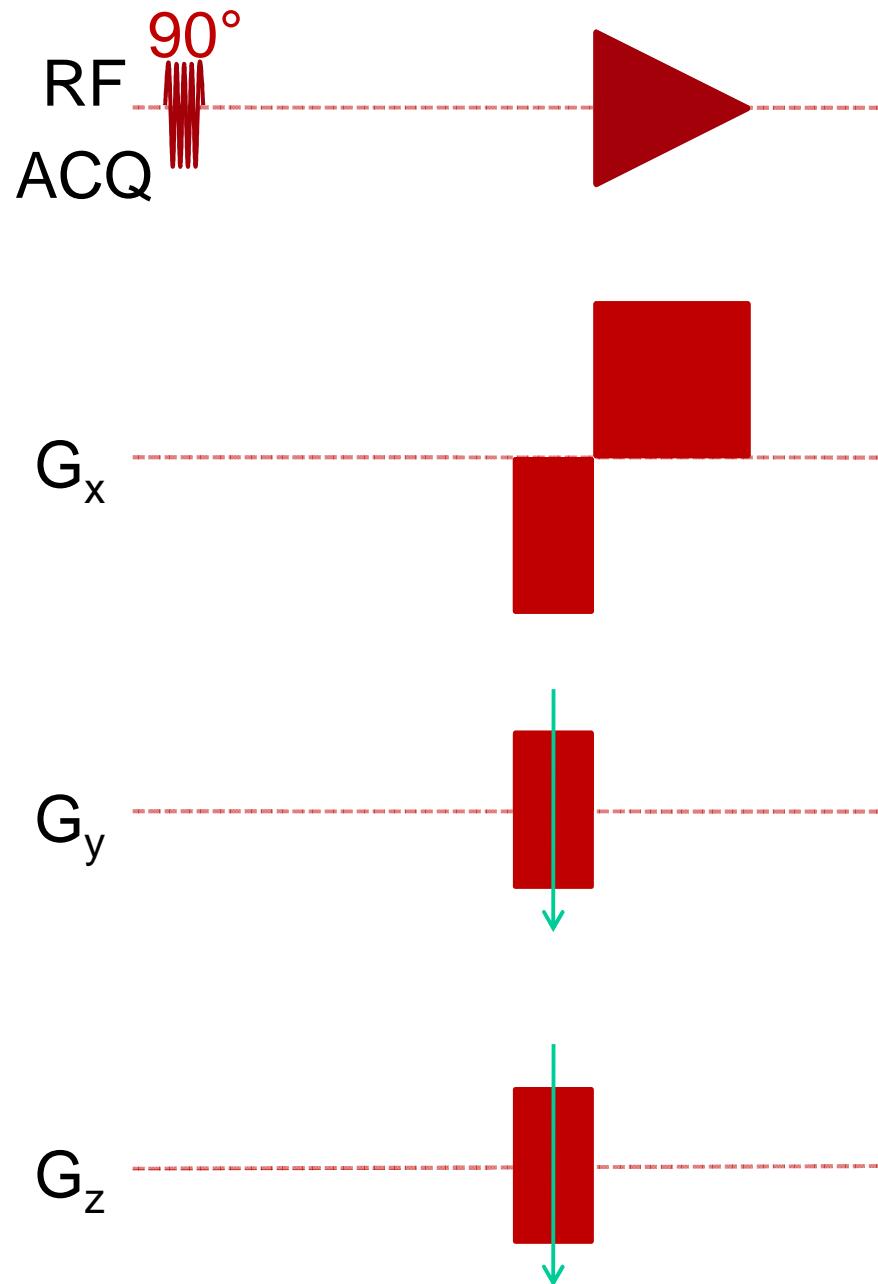
Temps d'acquisition

$$TA = 64^3 \times 1\text{s} = 73 \text{ h}$$

$$TA = N_x N_y N_z TR$$







# *Encodage Spin Warp*

Balayage Cartésien de l'espace k

Gradient pendant l'acquisition

Gradient de lecture

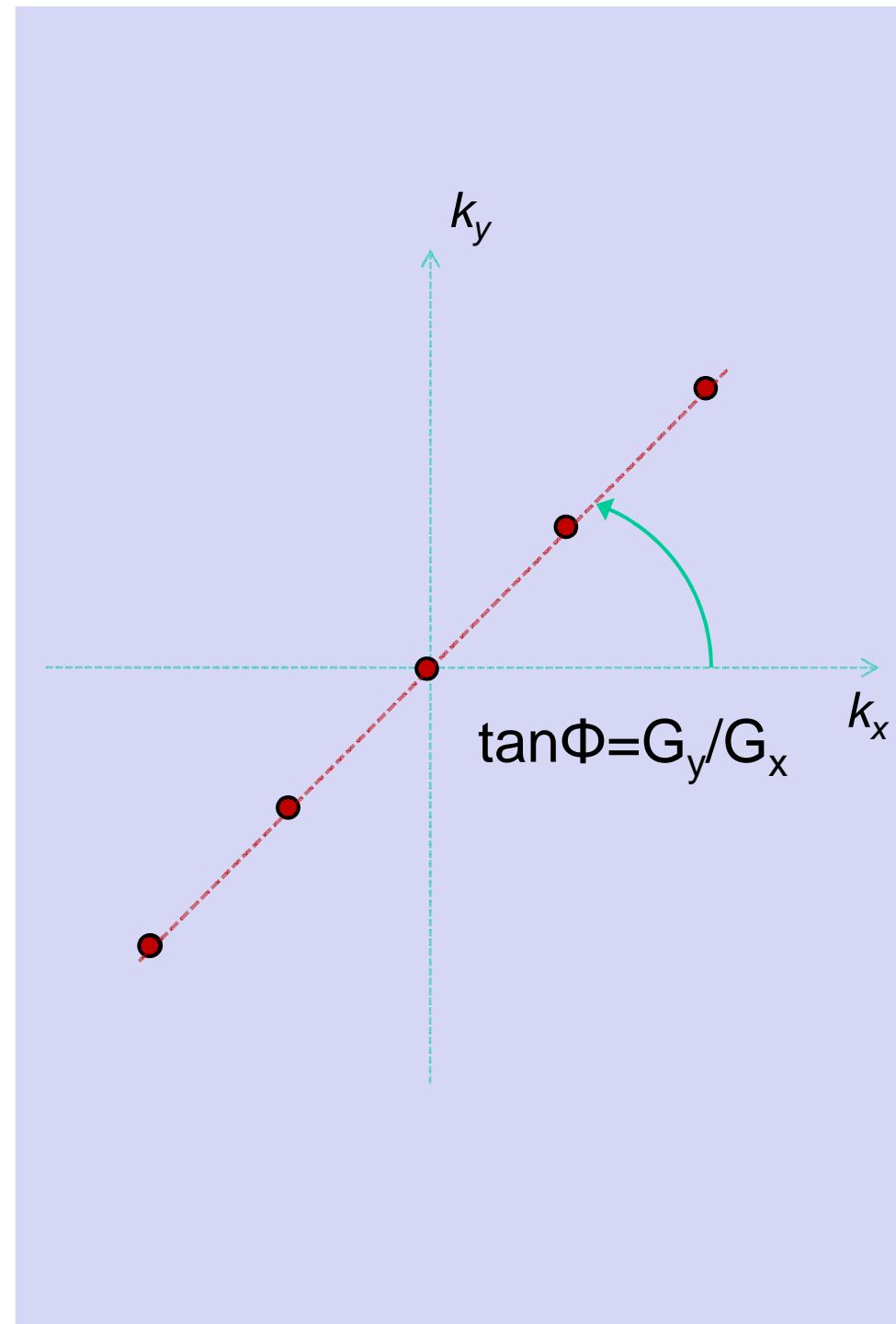
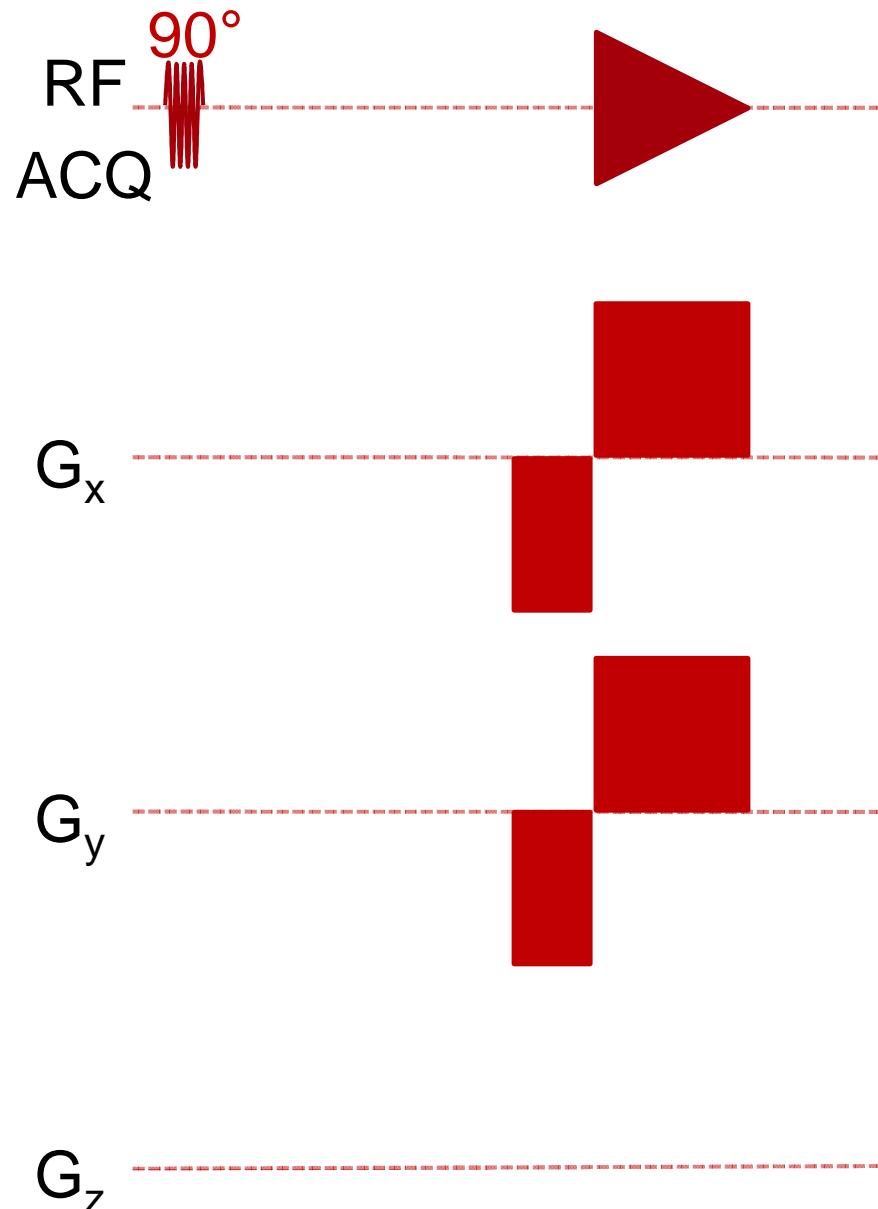
Une direction

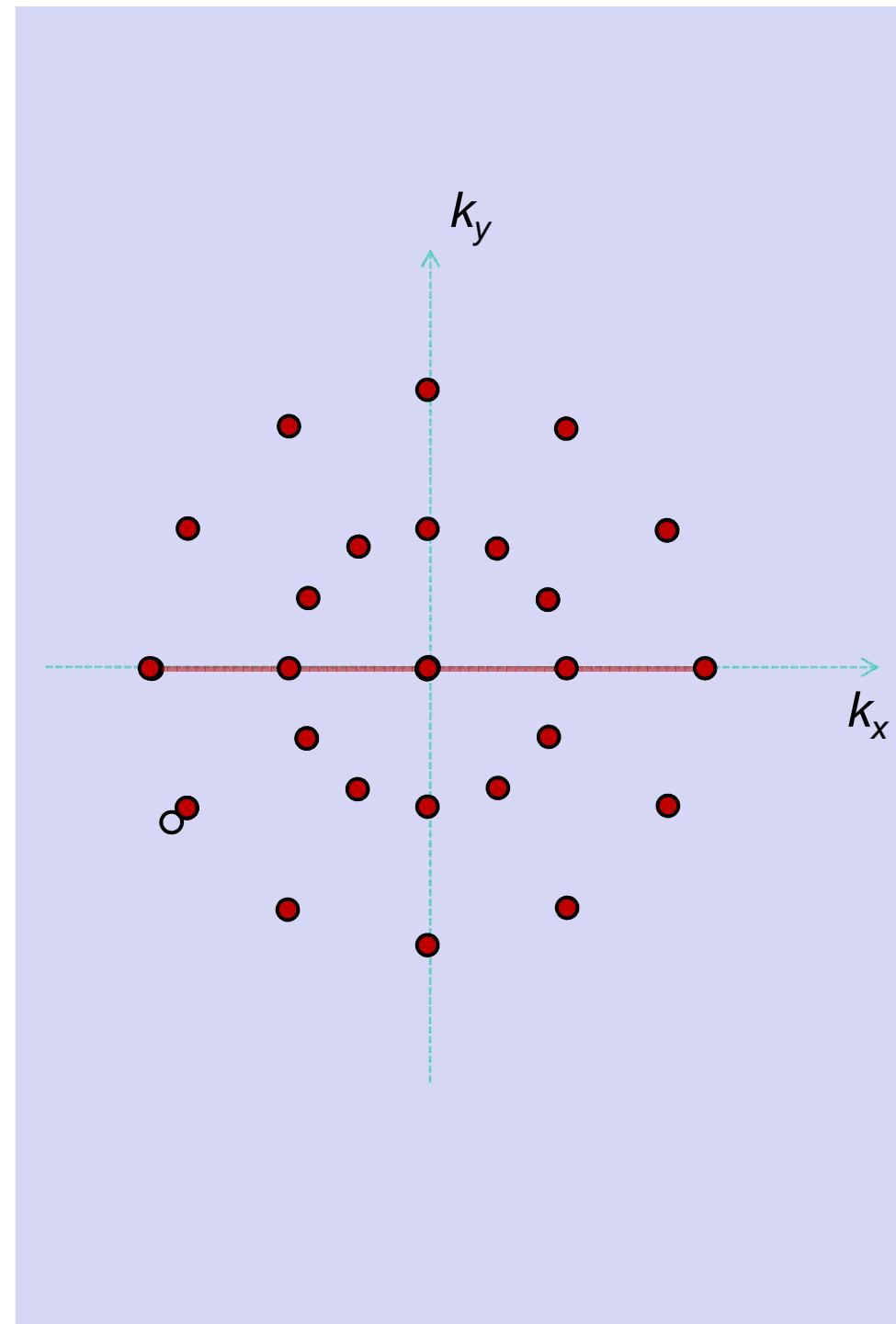
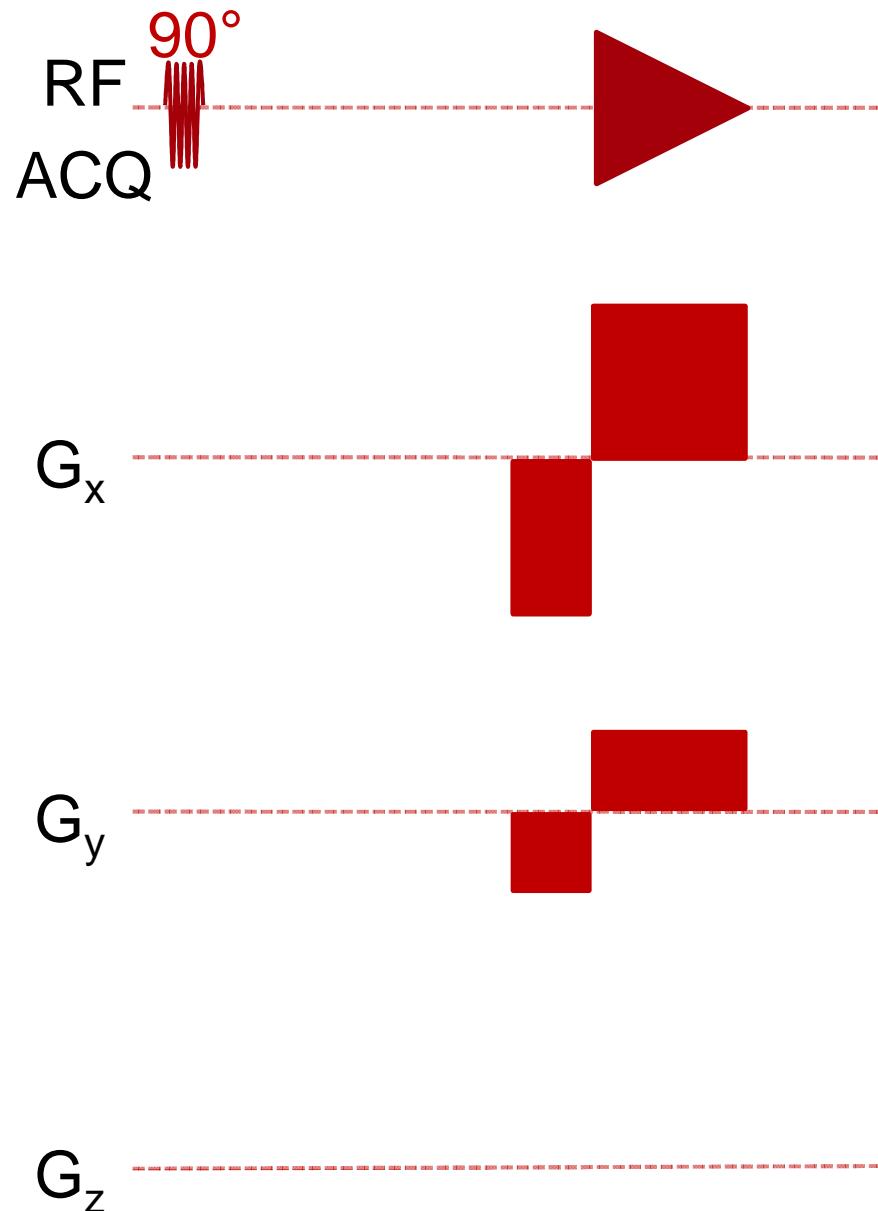
Gradient de codage de phase

Autres directions

Temps d'acquisition

$$TA = N_y (N_z)TR$$





# Encodage par projection

Balayage radial de l'espace k

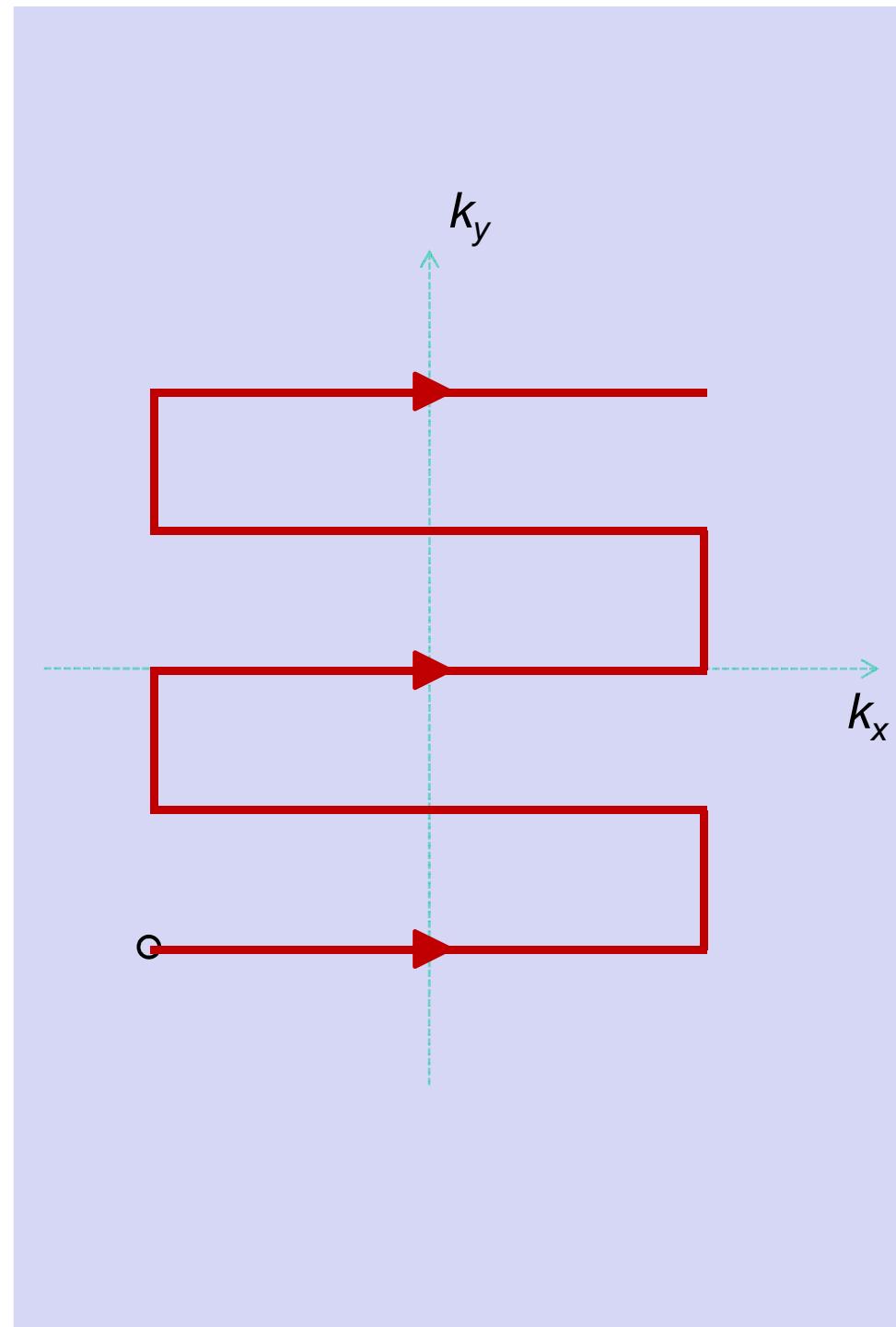
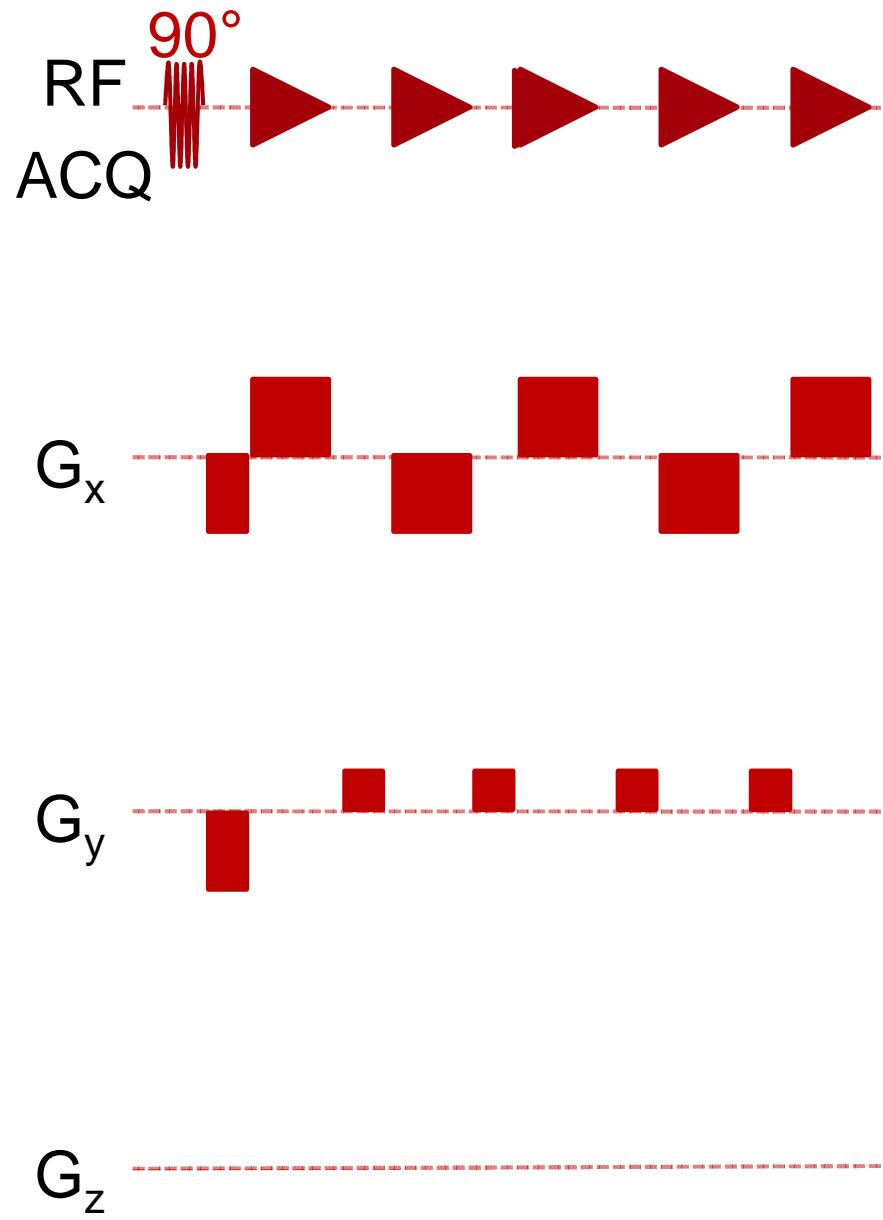
Gradient pendant l'acquisition

Gradient de lecture

Pas de gradient de codage de phase

Temps d'acquisition

$$TA = N_\phi (N_\theta) TR$$



# Encodage *echo planar*

Balayage cartesien de l'espace k

Gradient de lecture alterné

Incrément (blip) entre les phases de lecture

Temps d'acquisition                   $TA = TR$

Imagerie rapide



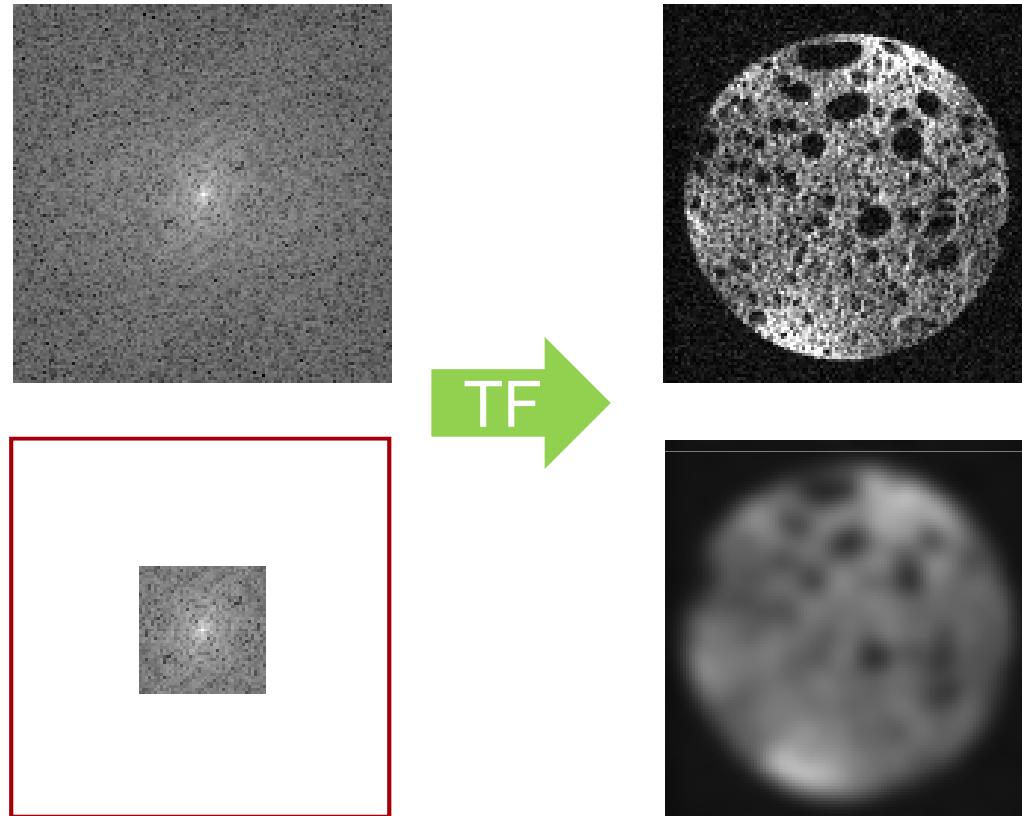
# Conséquences du remplissage dans l'espace réciproque



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# Résolution spatiale



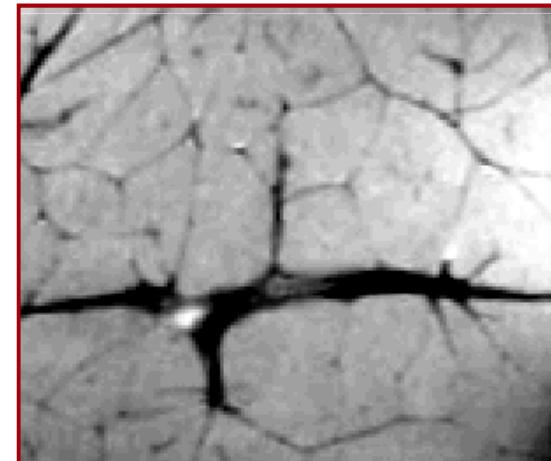
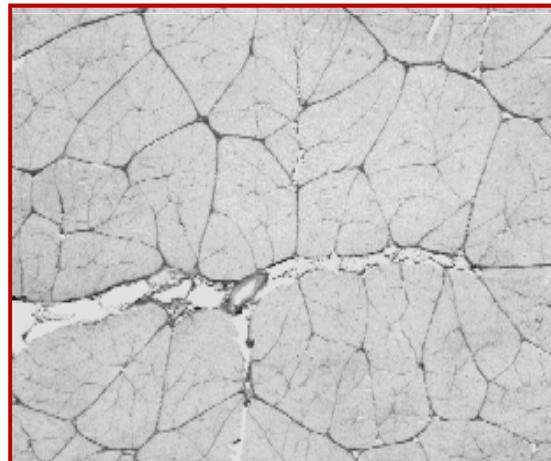
# Résolution spatiale

Domaine fréquentiel (espace k) à support limité

Résolution spatiale

$$\mathbf{k}_{\max} = \frac{\gamma}{2\pi} \int_0^T \mathbf{G}(t') dt'$$

Amplitude des gradients / Temps de commutation





# Sélection de coupe



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# Principe d'une sélection de tranche

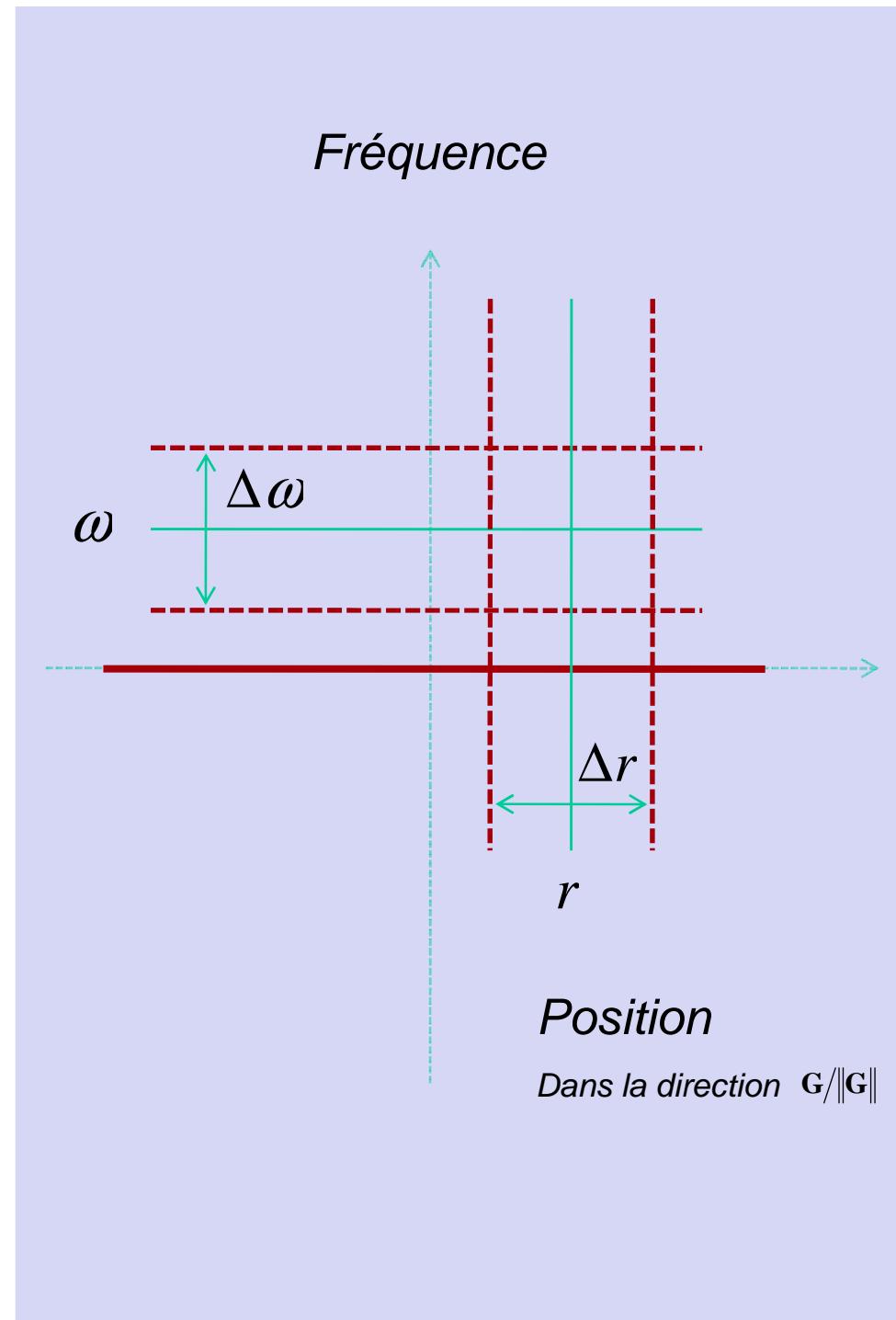
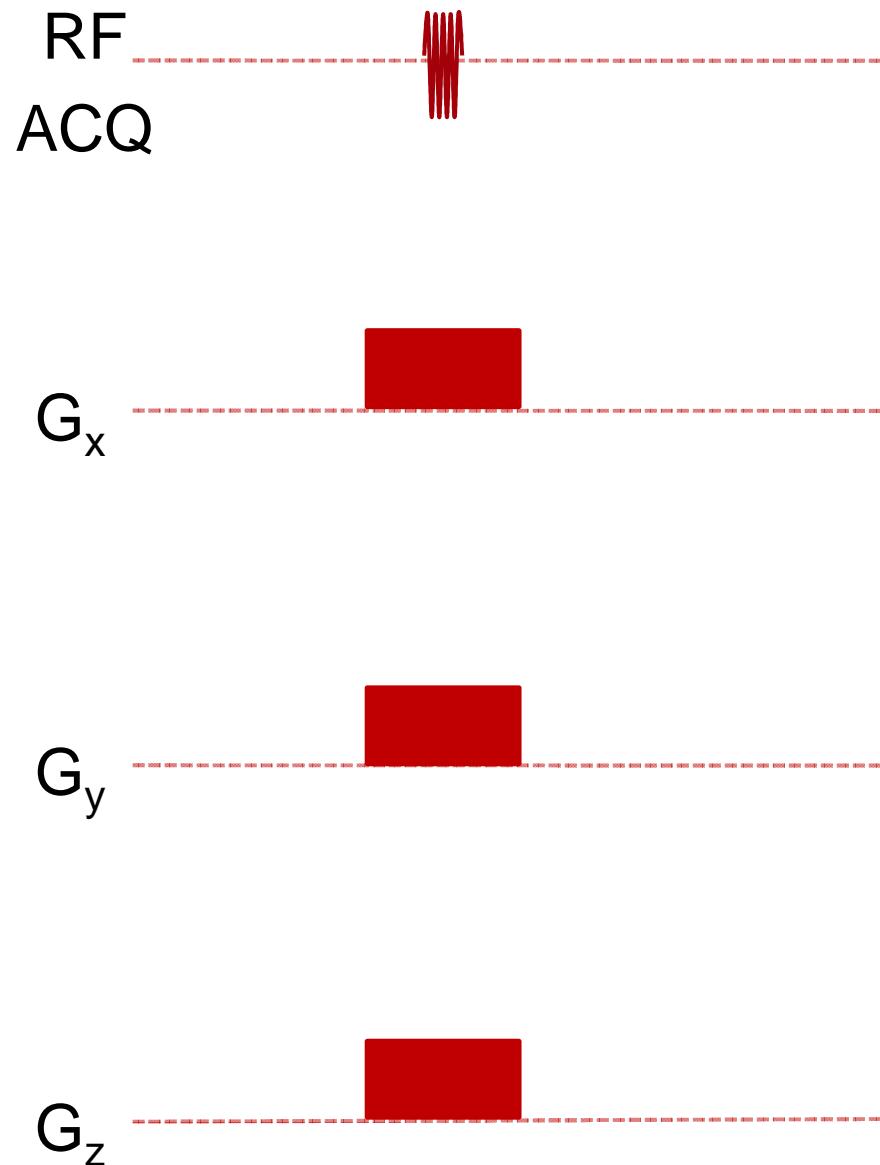
Excitation sélective d'une coupe épaisse

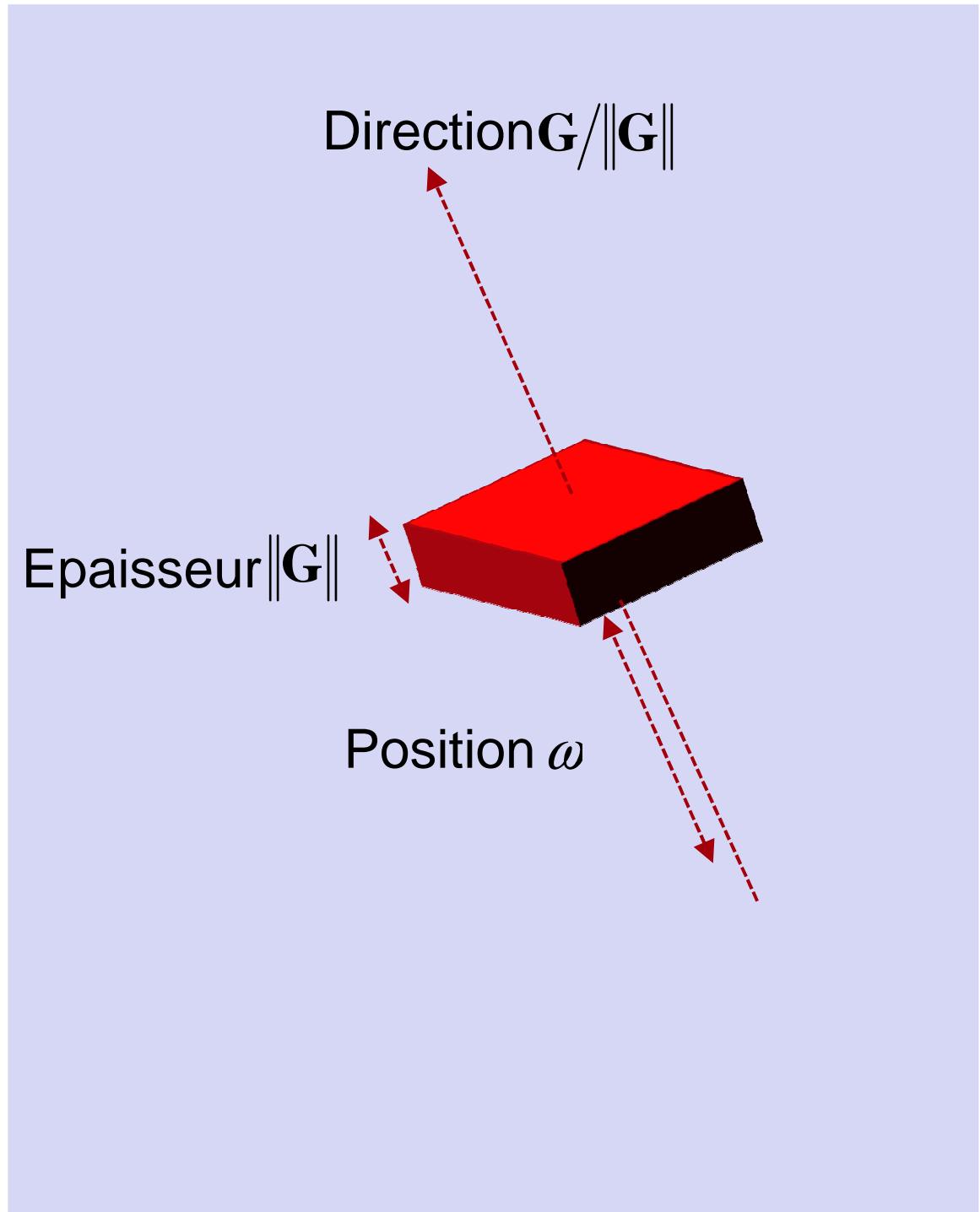
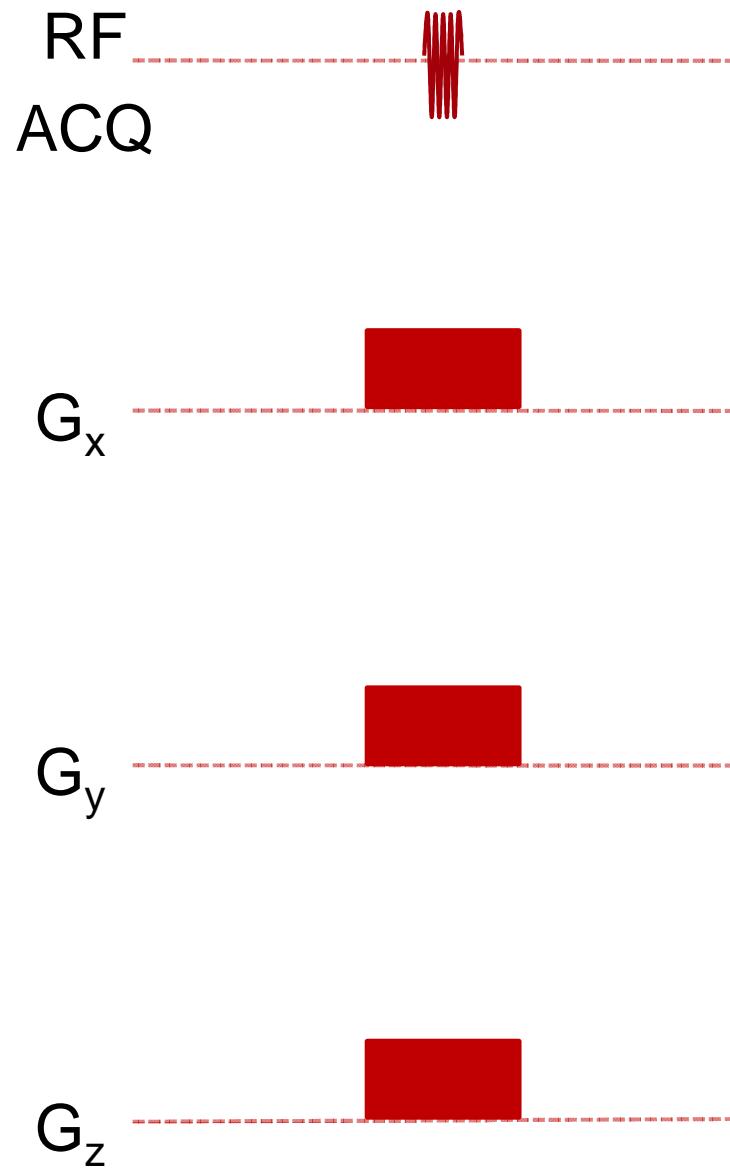
Application d'un gradient constant

Direction  $\mathbf{G}/\|\mathbf{G}\|$   
Amplitude  $\|\mathbf{G}\|$

Impulsion RF sélective en fréquence

Fréquence centrale  $\omega$   
Bande-Passante  $\Delta\omega$







## Synthèse et conclusions



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# Synthèse et conclusions

## Impulsions sélectives

Problème inverse

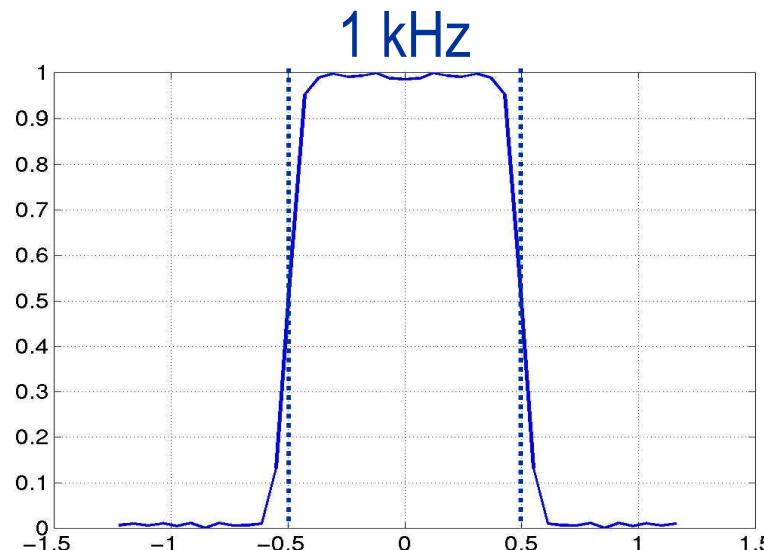
Formes algébriques prédéterminées

Transformées existantes

$B_1(t) \rightarrow M_T(\omega)$

Gauss, Sinc, Sech (...)

SLR, IST



# Synthèse et conclusions

Outils permettant de décrypter le codage spatial de 99% des séquences d'imagerie :

Balayage de l'espace k

Sélection de tranche

## Séquences 2D

X      Sélection de tranche

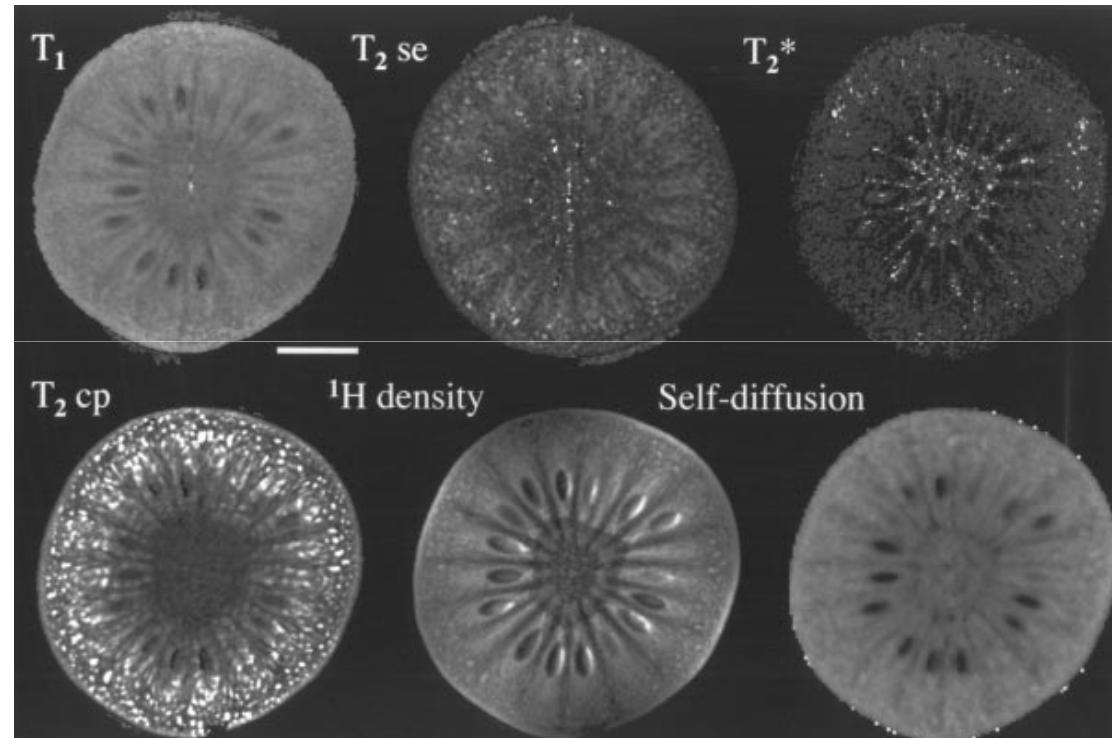
Y/Z    Balayage de l'espace k

## Séquences 3D

X/Y/Z    Balayage de l'espace k

# Synthèse et conclusions

Ajout de gradients et d'impulsions pour manipuler le contraste



Clark et al, *J Sci Food Agric* (1998)



# Références



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# Encodage

## Article princeps

Lauterbur

Image Formation by Induced Local Interactions: Examples Employing Nuclear Magnetic Resonance.

*Nature* 242, 190–191 (1973)

## Constant Time Imaging

Gravina, Cory

Sensitivity and resolution of constant-time imaging.

*J. Magn. Reson. B.* 104, 53-61 (1994)

## Chemical Shift Imaging

Brown, Kincaid, Ugurbil

NMR chemical shift imaging in three dimensions.

*Proc Natl Acad Sci U S A.* 79, 79 (1982)

## Spin Warp

Edelstein, Hutchison, Johnson, Redpath

Spin warp NMR imaging and applications to human whole-body imaging.

*Phys Med Biol.* 25, 751-756 (1980)

# Encodage

## Imagerie de projections

Bergin, Pauly, Macovski

Lung parenchyma : Projection reconstruction MR imaging

*Radiology* 179, 777-781 (1991)

## Echo Planar

Mansfield

Multi planar image formation using NMR spin echoes

*J Phys C* 3, L55-L58 (1977)

## Espace k

Twieg

The k space trajectory formulation of the NMR imaging process with applications in the analysis and synthesis of imaging methods

*Med. Phys.* 54, 338-343 (1983)

# Impulsions sélectives

## Fourier / Petits angles

Hoult

The solution of the bloch equations in the presence of a varying B1 field-An approach to selective pulse analysis

*J Magn Reson* 35, 69-86 (1979)

## Sech / Passages adiabatiques

Silver, Joseph, Hoult

Highly selective  $\pi/2$  and  $\pi$  pulse generation

*J Magn Reson* 59, 347-351 (1984)

## Transformée de Shinnar/LeRoux (SLR)

Pauly, LeRoux, Nishimura, Macovski

Parameter relations for the Shinnar-LeRoux selective excitation pulse design algorithm

*IEEE Trans. Med. Imaging* 10, 53-65 (1991)

## Mise en œuvre pratique SLR

Matson

An integrated program for amplitude-modulated RF pulse generation and re-mapping with shaped gradients

*Magn. Reson. Imaging* 12, 1205-1225 (1994)